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(Article begins on next page)

Comparative effects of metal oxide nanoparticles on human airway epithelial cells and macrophages

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Abstract Among nanomaterials of industrial relevance, metal-based nanoparticles (NPs) are widely used, but their effects on airway cells are relatively poorly characterized. To compare the effects of metal NPs on cells representative of the lung-blood barrier, Calu-3 epithelial cells and Raw264.7 macrophages

were incubated with three industrially relevant preparations of TiO₂ NPs (size range 4–33 nm), two preparations of CeO₂ NPs (9–36 nm) and CuO NPs (25 nm). While Raw264.7 were grown on standard plasticware, Calu-3 cells were seeded on permeable filters, where they form a high-resistance monolayer, providing an in vitro model of the airway barrier. Metal NPs, obtained from industrial sources, were characterized under the conditions adopted for the biological tests. Cytotoxicity was assessed with resazurin method in both epithelial and macrophage cells, while epithelial barrier permeability was monitored measuring the trans-epithelial electrical resistance (TEER). In macrophages, titania and ceria had no significant effect on viability in the whole range of nominal doses tested (15–240 µg/cm² of monolayer), while CuO NPs produced a marked viability loss. Moreover, only CuO NPs, but not the other NPs, lowered TEER of Calu-3 monolayers, pointing to the impairment of the epithelial barrier. TEER decreased by 30 % at the dose of 10 µg/cm² of CuO NPs, compared to untreated control, and was abolished at doses ≥80 µg/cm², in strict correlation with changes in cell viability. These results indicate that (1) CuO NPs increase airway epithelium permeability even at relatively low doses and are significantly toxic for macrophages and airway epithelial cells, likely through the release of Cu ions in the medium; (2) TiO₂ and CeO₂ NPs do not affect TEER and exhibit little acute toxicity for airway epithelial cells and macrophages; and (3) TEER measurement can provide a simple method to assess the impairment

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of in vitro airway epithelial barrier model by manufactured nanomaterials.

Keywords Copper oxide · Titanium oxide · Cerium oxide · Airway epithelium · Nanoparticles

Introduction

Among engineered nanomaterials, several metal-oxide nanoparticles (NPs) are extensively employed in industrial and commercial applications. Titanium dioxide (TiO₂) NPs occupy the first position in terms of economic importance within the range of metal oxide NPs and are used as pigments in painting industry for their photocatalytic properties (self-cleaning, antibacterial and anti-polluting action) and as sunblocking filter in cosmetics. Due to their antibacterial properties, copper oxide (CuO) NPs are utilized in many products of common use, such as inks, lubricants and coatings. Cerium dioxide (CeO₂) is currently used as diesel fuel additive, as component in fuel cells and as UV filter in cosmetics.

The exponential increase in metal NPs diffusion requires an in depth knowledge of their toxic properties. Since a variety of physico-chemical parameters of metal NPs, such as size, crystalline structure, chemical composition, surface area, biopersistence, capability to induce oxidative stress, have been considered as main factors for their toxicity, it is very difficult to foresee the toxic effect of newly synthesized NPs. Moreover, it is mandatory to take into account the specific endpoint that may depend on the biological model adopted.

As far as in vitro tests of toxicity are concerned, endpoints may be classified in cell specific and non-cell specific. The endpoints of the second type, such as loss of cell viability, apoptosis induction and genotoxicity, are relevant for almost all the cell models adoptable, although each cell type may have a specific sensitivity to a given nanomaterial (Sayes et al. 2007; Soto et al. 2007; Malugin et al. 2011). On the contrary, alterations in cell-specific functions, possibly of greater toxicological relevance, can be studied only in proper cell types.

Comparative studies may be very useful in characterizing the toxic properties of newly synthesized metal NPs (Lanone et al. 2009; Kroll et al. 2011), avoiding the problematic interpretation of investigations carried on a single NP in a particular cell type and providing relative toxicity indexes. To this purpose,

we have undertaken a pilot study on the effects of titanium oxide, cerium oxide and copper oxide NPs on cell-specific and not specific endpoints. We have used Calu-3 epithelial cells and Raw264.7 macrophages, two-cell models representative of, respectively, airway epithelium and macrophages. As for the cell models, Raw264.7 macrophages are a very commonly used macrophage model in toxicological studies on nanomaterials. Airway macrophages are specialized for interacting with inhaled particles and their exposure to NPs may lead to distinct types of macrophage activation, which account for different pathologic outcomes. On the other hand, Calu-3 cell line is a representative model of a tight airway epithelium, increasingly used in permeability studies. Airway epithelial cells represent the first anatomical barrier for inhaled NPs, and the contact between the nanomaterials and the epithelium may be prolonged, especially if phagocytosis is impossible or frustrated. Moreover, damage or dysfunction of the epithelial barrier may increase NPs access to lung interstitium and systemic circulation. As non-cell-specific endpoint, we have assessed alterations in cell viability, determined with a standard biochemical method, while, as an example of cell-specific endpoint, we have studied changes in the barrier function of airway epithelial cells.

Materials and methods

Cells

Calu-3 cells, obtained from a human lung adenocarcinoma and derived from serous cells of proximal bronchial airways (Finkbeiner et al. 1993), were obtained from the Istituto Zooprofilattico Sperimentale della Lombardia ed Emilia-Romagna (Brescia, Italy). Cells were routinely cultured in 10-cm diameter dishes in Eagle's Minimum Essential Medium (EMEM) supplemented with 1 mM sodium pyruvate, 10 % FBS, streptomycin (100 µg/mL) and penicillin (100 U/mL) in a humidified atmosphere of 5 % CO₂ in air. For permeability experiments, Calu-3 cells were seeded into cell culture inserts with membrane filters (pore size of 0.4 µm, Cat. No. 3095, Becton, Dickinson & Company, Franklin Lakes, NJ, USA) for 24-well multitrays, at a density of 75×10^3 cells/250 µL. Before the permeability experiments, cells were allowed to grow until a value of TransEpithelial

Table 1 Physicochemical features of target nanomaterials

NPs	Phase distribution (XRD)	SSA (BET, m ² /g)	Water dispersion ^a		i.e.p. ^b
			pH	Z pot (mV)	
TiO ₂ 1	Anatase 84 % Brookite 16 %	251	4.8	−28.6	2.3
TiO ₂ 2	Anatase 83 % Rutile 17 %	53	3.3	+59.3	4.8
TiO ₂ 3	Anatase 93 % Rutile 7 %	93	2.3	+66.1	4.1
CeO ₂ 1	CeO ₂ > 99.9 %	40	5.2	−4.9	5.0
CeO ₂ 2	CeO ₂ > 99.9 %	12	4.9	−25.5	2.6
CuO	CuO 86 % Cu ₂ O 14 %	25	4.8	+73.5	9–10 ^c

^a Concentration 1 mg/mL, pH for medium dispersion around 7.5

^b i.e.p. isoelectric point, pH value where Z potential is neutralized (0 mV)

^c From the literature data (Kittaka and Morimoto 1980)

Electrical Resistance higher than 1,000 Ω cm² was obtained. For cytotoxicity experiments, whenever not otherwise specified, cells were grown on 24-well plates (Falcon Cat. No. 3047, Becton, Dickinson & Company).

Raw264.7 macrophages were obtained from the Istituto Zooprofilattico Sperimentale della Lombardia ed Emilia-Romagna and routinely cultured in 10-cm diameter dishes in RPMI1640 medium supplemented with 10 % FBS and antibiotics. For the experiments, cells were seeded on 96-well microplates (Falcon Cat. No. 3072).

Characterization of nanoparticles

The panel of metal oxide NPs used consisted of: (a) three preparations of TiO₂ NPs synthesized for industrial applications [from Colorobbia, Montelupo Fiorentino FI Italy (TiO₂ 1), Evonik Degussa GmbH—Aeroxide P25 (TiO₂ 2), and Thetis SpA, Milan, Italy (TiO₂ 3)]; (b) two preparations of CeO₂ NPs (CeO₂ 1 and 2, both from Nanostructured & Amorphous Materials Inc., Houston, Texas, USA), and (c) CuO NPs (from Intrinsic Materials Inc., Rochester, NY, USA). TiO₂ 2 and 3 were used as received from the manufacturers, while TiO₂ 1, purchased as stable nanosol, was dried by spray-drying in order to be processed for toxicological tests. The main characteristics of the NPs used are summarized in Table 1, while the methods adopted for their characterization are detailed below.

Particle size distribution, based on hydrodynamic diameter, was evaluated by dynamic light scattering (DLS) technique. A nanometric particle size analyzer, Zetasizer Nano S (Malvern Instruments, Malvern, Worcestershire, UK) was used; scattering data were recorded at 25 ± 1 °C in backscattering modus at a scattering angle of 2 h = 173°. Each result corresponds to the average of five measurements, and each measurement is averaged within 15 performed analyses. Hydrodynamic diameter includes the coordination sphere and the species adsorbed on the particle surface such as stabilizers, surfactants, and so forth. DLS analysis provides also a polydispersion index (PDI), ranging from 0 to 1, to quantify the colloidal dispersion degree; for PDI lower than 0.3 samples may be considered monodispersed. Stock solutions (1 mg/mL) were ultrasonicated for 15 min and diluted to 0.1 mg/mL, both in water and RPMI1640 medium. DLS analyses were performed on both the diluted solutions.

The Zeta potential of stock solutions was measured by an electroacoustic technique (AcoustoSizer II Colloidal Dynamics, Sydney, Australia) based on the measure of the Electrokinetic Sonic Amplitude (ESA) signal generated in the colloidal systems. The ESA signal is an electrokinetic effect, generated by the motion of charged particles dispersed in a liquid when an alternate electric field is applied, that is related to the Zeta potential according to the theory developed by O'Brien et al. (1995). Moreover the system is equipped with an automatic pH titrating system used to

determine the Zeta potential of nanosols as a function of pH and to detect the isoelectric point (i.e.p), corresponding to a Zeta value of 0 mV. The analyses were performed on stock solutions (1 mg/mL).

The specific surface area (SSA) was determined by BET single point method (Brunauer et al. 1938) with a Sorpt 1750 apparatus (Carlo Erba, Milano, Italy). For spherical shape powder particles, it is possible to calculate one of the following parameters linked by a simple geometric relationship (German and Park 2008):

$$SSA = \frac{Area_{tot}}{M_{tot}} = \frac{n \cdot \pi \cdot \phi^2}{n \cdot 1/6 \cdot \pi \cdot \phi^3 \cdot \rho} = \frac{6}{\phi \cdot \rho}$$

where, SSA is the specific surface area (m²/g), ϕ is the particle mean diameter (μ m), and ρ is the powder density (g/cm³)

Applying this relationship, it was possible to calculate the particle mean diameter from SSA, to compare it with hydrodynamic diameter (DLS), aggregate size (SEM) and crystallite size (XRD) and to make some hypothesis on the morphology of primary particles and aggregates.

The XRD analysis allowed an estimation of amount of different phases present into the powder samples. Analyses were performed by a D500 diffractometer (Siemens, Munich, Germany), operating with Ni-filtered Cu K α radiation (35–52° 2 θ range, 0.02 s⁻¹, 3 s time-per-step). A Reference Intensity Ratio (RIR) was applied, basing upon scaling all diffraction data to the diffraction of standard reference materials (scale factor defined by: Intensity Analyte/Intensity Corundum = I/I_c).

Nickel nanoparticles (Byrne et al. 2009; Poland et al. 2011) were used as positive controls in cytotoxicity experiments.

Experimental treatments

Before the experiments, metal NPs were heated at 220 °C for 3 h to eliminate possible contamination from lipopolysaccharide. After cooling at room temperature, nanomaterials were dispersed at a concentration of 2 mg/mL in sterile phosphate-buffered saline (PBS). Immediately before experiments, the stock suspensions were extensively vortexed and sonicated for 15 min in a Branson Ultrasonic ultrasound bath. Stocks were used for no more than five experiments and maintained frozen in the

intervals among the experiments. NPs were added to normal growth medium to reach the desired dose. Taking into account the volume/surface ratio of the various culture systems adopted and the use of sub-confluent (cytotoxicity) or confluent monolayers (permeability studies), we have expressed the nominal doses as μ g of materials per cm² of monolayer.

Viability

Cell viability was assessed by the resazurin method (O'Brien et al. 2000). According to this method, viable cells reduce the non-fluorescent compound resazurin into the fluorescent resorufin that accumulates into the medium. After the exposure to NPs, carried on in thermostat, cells were incubated for 1 h with fresh, serum-free medium supplemented with 44 μ M resazurin; fluorescence was then measured at 572 nm with a fluorimeter (Wallac 1420 Victor2 Multilabel Counter, Perkin Elmer, Waltham, MA, USA).

For Calu-3 monolayers grown in a double chamber culture system, resazurin was added at both sides of the monolayer and fluorescence was measured in the apical compartment (Rotoli et al. 2009). Since NPs may interfere with the adopted viability method, the possible interference of the metal NPs with resorufin fluorescence has been excluded in preliminary experiments, according to the protocol previously adopted for MultiWalled Carbon Nanotubes (Rotoli et al. 2008).

Viability was also assessed through the direct observation of treated cultures by light microscopy, evaluating cell density and the presence of morphological alterations, such as cell rounding. Images of cells in phase contrast were obtained with a Nikon DS5MC digital camera (Nikon Instruments SpA, Firenze, Italy).

ROS generation

ROS generation was measured by a fluorometric assay using 5-(and-6)-chloromethyl-2',7'-dichlorodihydrofluorescein diacetate, acetyl ester (CM-H₂DCF-DA, Cat. No. C6827, Molecular Probes, Invitrogen, Grand Island, NY, USA). After the experimental treatments, cells were incubated with the probe (5 μ M) for 40 min. Cells were then washed and the fluorescence in cells was visualized using a fluorescence microscope (Nikon, Tokyo, Japan). Cells were then scraped, lysed in RIPA buffer (RadioImmunoPrecipitation Assay buffer, a buffer commonly used to lyse mammalian

Table 2 Comparison between particle size assessed by different techniques

	Mean hydrodynamic diameter (DLS, nm/PDI) ^a		Phase, crystallite size (nm)		Equivalent spherical diameter (BET, nm)	Aggregate size (SEM, μm)
	Water	Medium				
TiO ₂ 1	266/0.6	609/0.8	Anat., 4	Brook., 4	6	≈ 5
TiO ₂ 2	360/0.3	1,090/0.7	Anat., 22	Rutile, 33	30	≈ 3
TiO ₂ 3	2,135/0.4	1,770/0.4	Anat., 16	Rutile, 20	17	≈ 20
CeO ₂ 1	1,280/0.9	1,685/0.9	CeO ₂ , 9		20	–
CeO ₂ 2	133/0.8	746/0.9	CeO ₂ , 36		65	–
CuO	283/0.3	1,200/0.6	CuO, 25		24	–

PDI polydispersity index. PDI < 0.3 monodispersed suspension, PDI > 0.3 polydispersed suspension

^a Concentration 0.1 mg/mL

Fig. 1 SEM micrographs of TiO₂ 1 (*left*), TiO₂ 2 (*middle*) and TiO₂ 3 (*right*) samples

cells: 20 mM Tris–HCl (pH 7.5); 150 mM NaCl, 1 mM Na₂EDTA; 1 mM EGTA; 1 % NP-40; 1 % sodium deoxycholate; 2.5 mM sodium pyrophosphate; 1 mM β -glycerophosphate; 1 mM Na₃VO₄; 1 $\mu\text{g}/\text{mL}$ leupeptin, pulse sonicated for 15 s and centrifuged at $12,000\times g$ for 15 min at 4 °C, and fluorescence was measured with a Wallac Victor2 microplate reader. Before centrifugation, an aliquot of lysate was used to determine protein content with the method of Bradford. The intensity of fluorescence was expressed as Arbitrary Units (AU) per μg of protein.

To estimate ROS generation in acellular systems, the probe (5 μM) was added to growth medium supplemented with the NPs, and fluorescence was read with a Wallac Victor2 microplate reader after 60 min of incubation.

Trans-epithelial electrical resistance (TEER)

For measurements of TransEpithelial Electrical Resistance (TEER) Calu-3 cells were seeded into cell culture inserts with membrane filters (pore size of 0.4 μm) for

Falcon 24-well-multitrays (Cat. No. 3095, Becton, Dickinson & Company, Franklin Lakes, NJ, USA), at a density of 75×10^3 cells/250 μl . Before the permeability experiments, cells were allowed to grow, usually for 10–14 days, until a value of TEER higher than $1,000 \Omega \text{ cm}^2$ was reached, indicating the formation of a tight epithelial layer. TEER measurements were made using an epithelial voltohmmeter (EVOM, World Precision Instruments Inc., Sarasota, FL, USA). Materials were added in the apical chamber from the stock solutions without changing the medium. TEER changes were expressed as the percentage of the initial value adjusted for control cell layers according to the equation (Salem et al. 2009).

$$\text{TEER \%} = \frac{\text{Final TEER}_{\text{treated}}}{\text{Final TEER}_{\text{control}}} \times \frac{\text{Initial TEER}_{\text{control}}}{\text{Initial TEER}_{\text{treated}}} \times 100$$

Statistics

Values of viability and TEER were analysed with ANOVA using post hoc Bonferroni test.

Fig. 2 Effects of metal oxide NPs on macrophage viability. Raw264.7, grown for 48 h in complete growth medium, were treated for 24 h with the indicated NPs. At the end of the incubation, cell viability was assessed with the resazurin method

(see ‘Materials and methods’ section). Data are means of five independent determinations with SD shown. The experiment was repeated twice with comparable results. *** $P < 0.01$ versus untreated, control cells

Reagents

FBS and culture media were purchased from Euro-Cclone SpA, Pero, Milan, Italy. Sigma-Aldrich (Milan, Italy) was the source of all other chemicals, whenever not specified otherwise.

Results

Physico-chemical characterization of NPs

The main characteristics of the NPs investigated are reported in Table 1, while information about particle

size is summarized in Table 2. All particles have a micrometric aggregate structure, evidenced by hydro-dynamic diameter—measured by DLS—and morphology—detected by SEM—similar to that shown in Fig. 1 for TiO_2 powders, and resulted polydispersed, with the exception of TiO_2 2 and CuO in water. Nevertheless, the aggregates have a primary nano-structure, as assessed by crystallite size and BET equivalent spherical diameter. These two techniques yielded comparable values, indicating the presence of discrete nanometric units with crystalline order that form the aggregate structure. The primary particle size of investigated powders is about 20.0–30.0 nm, with

Fig. 3 Effects of CuO NPs on macrophage viability. Raw264.7, grown for 48 h in complete growth medium, were treated for 24 h (a) or 48 h (b) with the indicated doses of CuO NPs. At the end of the incubation, cell viability was assessed with the resazurin method (see ‘Materials and methods’ section). Data are means of five independent determinations with SD shown. The experiment was repeated three times with comparable results. *** $P < 0.01$ versus untreated, control cells

exception for TiO₂ 1 that shows the finest nanostructure (BET diameter of 6 nm) and CeO₂ 2 that shows the largest nanostructure (BET diameter of 65 nm).

An increase of the mean hydrodynamic diameters, associated to a lower colloidal stability, was observed for all the samples dispersed in RPMI1640 medium. Agglomeration phenomena detected passing from the water solution to the medium can be attributed to the higher ionic strength of the medium and to the presence of divalent (Ca^{2+} and Mg^{2+}) cations that shift the isoelectric point towards the more basic medium pH (Long et al. 2006).

CeO₂ suspensions showed the lowest degree of stability; in particular CeO₂ 1 suspension was completely precipitated after 1 h-settling (Supplementary

Fig. 1), in spite of the lower BET equivalent diameter than CeO₂ 2. The higher stability of CeO₂ 2 is justified by the more negative Zeta potential (-4.9 mV for CeO₂ 1, -25.5 mV for CeO₂ 2), due to the shift of isoelectric point from 5.0, for sample CeO₂ 1 [in agreement with (Mao et al. 2010)] to 2.6 for CeO₂ 2, far from its natural pH (4.9 vs. 5.2 for CeO₂ 1).

The detected difference between the isoelectric points of two different CeO₂ samples agrees with a trend observed in the literature for TiO₂ nano powders prepared with the same synthetic procedure but having different BET equivalent diameters, where a shift of isoelectric point towards more acidic region was detected at increasing primary particle sizes (Suttiponparnit et al. 2011).

For titania, the electroacoustic technique applied here has yielded, for TiO₂ 2 in water, an acid pH, probably due to residual synthesis byproducts and an i.e.p. of 4.8, with a Zeta potential at natural pH quite high ($+59.3$). A quite similar behaviour was detected for TiO₂ 3 sample, while TiO₂ 1 sample resulted negatively charged (-28.6 mV) at natural pH (4.8) with an isoelectric point of 2.3 justifiable by anionic species adsorbed into TiO₂ surface added during sol-gel synthesis. Nevertheless, the large aggregates (≈ 20 μm) of TiO₂ 3 sample, evidenced by SEM measurements justifies the higher sedimentation rate and the larger hydrodynamic diameters detected by DLS measurements.

The CuO natural pH of 4.8 (in water) is far enough from its isoelectric point, which ranges from 9 to 10 (Kittaka and Morimoto 1980), so as to ensure a relatively good colloidal stability.

Effects of metal NPs on the viability of Raw264.7 cells

Figure 2 (panels a–e) depicts the effects of TiO₂ and CeO₂ NPs on the viability of Raw264.7 cells in a dose range between 15.0 and 240.0 $\mu\text{g}/\text{cm}^2$ of monolayer (corresponding to 22.5 and 360 $\mu\text{g}/\text{mL}$ in the culture system adopted). No significant loss of viability was recorded with any NP. On the contrary, CuO NPs (Fig. 2f) had very marked effects on cell viability, comparable to that observed upon treatment with Ni NPs, used as a positive control (Panel g).

A similar experiment, performed in a lower range of doses of CuO NPs (Fig. 3), indicated significant toxicity at doses ≥ 5.0 $\mu\text{g}/\text{cm}^2$ after 24 h of exposure

Fig. 4 Effects of metal oxide NPs on macrophage viability. Raw264.7 cells were incubated for 24 h in growth medium in the absence (**a** control) or in the presence of the following NPs: Nickel (30 $\mu\text{g}/\text{cm}^2$, **b** positive control), TiO_2 1 (80 $\mu\text{g}/\text{cm}^2$ **c**), TiO_2 2 (80 $\mu\text{g}/\text{cm}^2$ **d**), TiO_2 3 (80 $\mu\text{g}/\text{cm}^2$ **e**), CeO_2 1 (80 $\mu\text{g}/\text{cm}^2$

f), CeO_2 2 (80 $\mu\text{g}/\text{cm}^2$ **g**) and CuO (20 $\mu\text{g}/\text{cm}^2$ **h**). At the end of the incubation, cultures were observed in phase contrast. Images of representative field are shown. The experiment was repeated two times with comparable results

while, at 48 h, even the lowest dose employed (2.5 $\mu\text{g}/\text{cm}^2$) caused a significant viability loss; macrophage viability was substantially suppressed after 24 h of exposure at doses $>10.0 \mu\text{g}/\text{cm}^2$ (corresponding to 15 $\mu\text{g}/\text{mL}$).

Microscopic observation was used to confirm the results of the biochemical test. Compared to untreated cultures (Fig. 4a), the positive control, consisting of Ni NPs, produced evident cell loss and rounding. On the contrary, TiO_2 and CeO_2 NPs did not markedly affect culture morphology, even if NP aggregates were clearly detectable on the monolayer surface (Fig. 4 c–g). Conversely, CuO NPs, at a dose of 20.0 $\mu\text{g}/\text{cm}^2$, produced an evident cell loss (Fig. 4h).

The effects of CuO NPs were compared with those of Cu^{++} ions (supplemented to the growth medium as CuCl_2) at equivalent doses of copper (Fig. 5). The results indicated that, at comparable Copper content in the assays, CuO NPs and CuCl_2 gave similar effects.

The induction of oxidative stress by the panel of selected NPs was then investigated in the experiments shown in Figs. 6 and 7. In the experiment shown in Fig. 6, the effect of the six NPs on the production of ROS, evaluated from the changes in carboxyfluorescein fluorescence, was assessed in the absence of cells, demonstrating that only CuO NPs produced a significant increase of fluorescence. Supplementation with the antioxidant *N*-acetyl-cysteine (NAC) significantly

Fig. 5 Comparison between the effects of CuCl₂ and CuO NPs on macrophage viability. Raw264.7 cells were incubated for 24 h (a) or 48 h (b) with increasing doses of CuCl₂ and CuO NPs, selected to cover a comparable range of copper concentrations (from 0 to 53.2 µg/cm² of copper for CuO NP, from 0 to 56.51 µg/cm² of copper for CuCl₂). At the end of the incubation, cell viability was determined with the resazurin method. Data are means of five independent determinations with SD. The experiment was performed twice with comparable results

reduced the fluorescence increase due to CuO NPs. When CuO NPs were added to the growth medium of Raw264.7 cells, a clear cut intracellular ROS production was evident from the increase in fluorescence detected in both cell lysates (Fig. 7a) and cells in situ (Fig. 7b). Consistently with a role of ROS in CuO NPs effects, the addition of NAC significantly protected Raw264.7 cells from the cytotoxicity induced by sub-maximal doses of this nanomaterial (Fig. 8).

Fig. 6 ROS production by metal oxide NPs in acellular systems. 100 µl of medium was supplemented with CM-H₂DCF-DA (5 µM) and 20 µg/cm² of the indicated NP for 60 min. H₂O₂ (2 mM) was added as a positive control. NAC *N*-acetyl-cysteine 2 mM. Fluorescence was determined after 60 min as described under 'Materials and methods' section. Data are means of four independent determinations with SD. The experiment was repeated three times with comparable results. ****P* < 0.01 versus untreated, control cells

Effects of metal NPs on the transepithelial electrical resistance in Calu-3 cell monolayers

After reaching confluence on membrane filters, Calu-3 monolayers develop progressively high transepithelial electrical resistance (TEER), forming a competent epithelial barrier. The addition of CuO NPs to the apical compartment of these monolayers had impressive effects on TEER. In the experiment shown in Fig. 9, CuO NPs were added to high-TEER, confluent monolayers. Control monolayers, not treated with the NPs, further increased TEER above the initial value. CuO NPs lowered TEER in a dose-dependent way. Indeed, after 2 days of exposure to 10.0 µg/cm² of CuO NPs, TEER of treated monolayers was already significantly lower than untreated counterpart (30 %) and at doses ≥80.0 µg/cm² TEER was abolished. Conversely, the other metal NPs had no apparent effect on TEER, given that, even when used at high doses (120 µg/cm²), neither TiO₂ nor CeO₂ NPs affected the resistance, even if the TEER of parallel monolayers was clearly affected by 40 µg/cm² of CuO NPs (Fig. 10). The relationship between cytotoxicity and epithelial barrier impairment was investigated studying in the same monolayers the effects on TEER and cell viability of low doses of CuO NPs (Fig. 11). The results indicate that there was a close association between viability lowering and TEER decrease.

Fig. 7 ROS production by metal oxide NPs in Raw264.7 cells. Upper Raw264.7 cells were incubated for 24 h in the absence (control) or in the presence of CuO NPs ($5 \mu\text{g}/\text{cm}^2$) or H_2O_2 (2 mM). At the end of the incubation, cells were incubated for 30 min with CM- $\text{H}_2\text{DCF-DA}$ ($5 \mu\text{M}$). Fluorescence was determined as described in ‘Materials and methods’ section. Data are means of three independent determinations with SD. The experiment was performed three times with comparable results. * $P < 0.05$, ** $P < 0.01$. Lower before determination of the intracellular CM- $\text{H}_2\text{DCF-DA}$, images of representative fields were taken in phase contrast (a–c) or with fluorescence microscope (d–f). a, d control, untreated cultures. b, e CuO NPs. c, f H_2O_2

Discussion

The main findings gathered by our study are the following: (i) CuO NPs exert dose dependent toxicity

Fig. 8 Protection of Raw264.7 from CuO NPs by antioxidants. Raw264.7 cells were incubated for 24 h with CuO NPs (5 or $10 \mu\text{g}/\text{cm}^2$) in the presence or in the absence of NAC (1 mM). At the end of the incubation, cell viability was assessed with the resazurin method. Control, cells treated with neither CuO NPs nor NAC. Data are means of five independent determinations with SD. The experiment was repeated three times with comparable results. *** $P < 0.01$ versus cells treated with the same dose of CuO NPs in the absence of NAC

on both macrophages and airway epithelial cells with comparable potency; (ii) in airway epithelial cell monolayers, the exposure to CuO NPs causes a dose-dependent, progressive TEER decrease, pointing to the impairment of the epithelial barrier; (iii) as a toxicity indicator, TEER is as sensitive as changes in cell viability, determined with biochemical methods. Actually, the results shown indicate a strict correlation between TEER decrease and viability loss; (iv) TiO_2 and CeO_2 NPs are not significantly toxic on macrophages and do not cause marked TEER changes in epithelial cell monolayers.

Copper oxide NPs have been consistently reported as being endowed with significant cytotoxicity (Karlsson et al. 2008; Lanone et al. 2009; Studer et al. 2010), and the results shown here clearly suggest that epithelial barrier perturbation must be included among the toxic effects of this nanomaterial. CuO NP cytotoxicity seems correlated to oxidative stress, since cell production of ROS is already evident at the lowest cytotoxic dose, and NAC exerts a significant protective role. The higher toxicity shown by CuO NPs in comparison with TiO_2 and CeO_2 powders can be related to the stability of CuO NPs dispersions, that are

Fig. 9 Effects of CuO NPs on the trans-epithelial electrical resistance (TEER) of Calu-3 cell monolayers. Confluent Calu-3 monolayers, grown for 13 days, were incubated in the presence of the indicated doses of CuO NPs, added at the apical side of the monolayer (Time 0). The trans-epithelial electrical resistance (TEER) was measured (see ‘Materials and methods’ section) on daily basis from the second to the fourth day of treatment. Data are values obtained from single monolayers and are expressed as % of the initial value (see ‘Materials and methods’ section). The experiment was repeated four times with comparable results

remarkably more stable compared to titania and ceria dispersions, and to their positive Z potential. Positive Z potential can affect toxicity mechanism, given that it is documented that cationic surfaces generally exert stronger effects than their anionic counterparts (Nel et al. 2009). However, at variance with what reported by others in A549 cells (Karlsson et al. 2008), a strict parallelism exists between the toxic effects caused by CuO NP and Cu^{++} ions (as CuCl_2), when doses are expressed on copper basis. While the reason for the divergent results reported by Karlsson et al. (2008) and us are not obvious, our data suggest that cytotoxicity by CuO NPs is in fact due to copper release, promoted by the organic components of the growth medium (Gunawan et al. 2011), rather than to a direct interaction between the NP and the biological system. Thus, cytotoxicity by CuO NPs should be referred, at least under the conditions adopted here, to the paradigm of chemical toxicity. However, nanosize may influence CuO NP toxicity determining leaching kinetics, as recently proposed by other authors (Gunawan et al. 2011).

Fig. 10 Effects of metal oxide NPs on the trans-epithelial electrical resistance (TEER) of Calu-3 cell monolayers. Confluent Calu-3 monolayers, grown for 10 days, were incubated in the presence of the indicated NPs at the dose of $120 \mu\text{g}/\text{cm}^2$ (for CuO NPs, $40 \mu\text{g}/\text{cm}^2$), added at the apical side of the monolayer. The trans-epithelial electrical resistance (TEER) was measured (see ‘Materials and methods’ section) after two (a) or seven days (b). Data are means of four independent determinations with SD from a representative experiment repeated twice with comparable results. *** $P < 0.01$ versus control, untreated monolayers

In contrast, titanium dioxide NPs have been extensively studied on various cell types and considered relatively poorly toxic (Lanone et al. 2009; George et al. 2011), although some studies report functional alterations, and even clear acute cytotoxicity, in macrophages and airway epithelial cells (Singh et al. 2007; Hussain et al. 2009; Fenoglio et al. 2009; Liu et al. 2011). Moreover, evidence for chronic toxic effects of titania in vivo has been established (IARC 2010; NIOSH 2011). In our experiments, very high

Fig. 11 Dose dependence of the effects of CuO NPs on TEER and viability of Calu-3 cell monolayers. Confluent Calu-3 monolayers, grown for 14 days, were incubated in the presence of the indicated doses of CuO NPs, added at the apical side of the monolayer. After seven days, trans-epithelial electrical resistance (a) and cell viability (b) were determined in the same monolayer. Data are means of three independent determinations with SD from a representative experiment repeated twice with comparable results. *, **, *** $P < 0.05$, 0.01 and 0.001, respectively, versus control, untreated monolayers

doses of titania of different crystalline phase do not cause significant cytotoxicity in either macrophages or airway epithelial cells and do not perturb epithelial permeability. Lack of toxicity cannot be due to limited sensitivity of the methods used, since cytotoxicity was readily detected with either CuO NPs or Ni NPs, used as a positive control. However, it should be stressed that failure to detect toxic effects may be due to particular conditions of the biological system (such as, for instance, cell type or density of the cell culture during the exposure) and that the absence of overt cytotoxicity does not exclude the possibility of subtler biological effects, such as, for instance, macrophage activation. More importantly, under our experimental

conditions, titania are endowed with poor colloidal stability and aggregate in lumps clearly detectable in the micrometric range (Fig. 4), thus preventing the interaction between true nanosized structures and the biological system.

Few toxicological studies on cerium oxide NPs have been published and no information is available on possible correlations between physico-chemical properties and toxic effect for this material. Such studies yielded conflicting results, indicating either cytotoxic (Lin et al. 2006; Xia et al. 2008; Ma et al. 2011) or protective effects (Rzagalinski et al. 2006; Celardo et al. 2011). In our hands, ceria NPs do not appear endowed with significant toxic effects, either on macrophage and airway epithelia viability or on the epithelial barrier. Also for these NPs, however, the same considerations developed above for titania are valid and further studies will be needed to ascertain possible effect on macrophage activation.

The data about effects on TEER of NPs are of particular interest, since they represent the first investigation in which this parameter is evaluated in epithelial cells exposed to metal-based nanomaterials. Interestingly, even at high doses, neither titania nor ceria seem to impair the epithelial barrier, although they have a clear cut tendency to form large aggregates on the monolayers. Conversely, for multi-walled carbon nanotubes, which cause a well-defined barrier impairment in the same biological model (Rotoli et al. 2008), aggregation tendency seems an important factor for the establishment of the toxic effect (Rotoli and Bussolati, unpublished observations). On the contrary, CuO NP exert a significant toxic effect on the epithelial barrier that closely parallels their effect on cell viability (Fig. 11).

In summary, the strict similarity between the dose-effect relationship of CuO for toxicity and TEER decrease suggests that TEER provides a simple and sensitive device for the evaluation of NP toxic effects in epithelial models. Moreover, this study confirms the low acute toxicity of titania and ceria and indicates that the high toxicity of CuO NPs may be related to the release of Cu^{++} ions and, hence, modulated by their rate of leaching from the NP.

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