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Effect of carbon fiber type on monotonic and fatigue properties of orthopedic grade PEEK

Keywords: PEEK composites; fatigue crack propagation; orthopedic biomaterials; fractography

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Abstract

- 1 2
- 3 Carbon-fiber reinforced (CFR) PEEK implants are used in orthopedic applications ranging from
- 4 fracture fixation plates to spinal fusion cages. Documented implant failures and increasing
- 5 volume and variety of CFR PEEK implants warrant a clearer understanding of material behavior
- 6 under monotonic and cyclic loading. To address this issue, we conducted monotonic and fatigue
- 7 crack propagation (FCP) experiments on orthopedic grade unfilled PEEK and two formulations
- 8 of CFR PEEK (PAN- and pitch-based carbon fibers). The effect of annealing on FCP behavior
- 9 was also studied. Under monotonic loading, fiber type had a statistically significant effect on
- 10 elastic modulus (12.5 ± 1.3 versus 18.5 ± 2.3 GPa, pitch versus PAN CFR PEEK, AVG \pm SD)
- and on ultimate tensile strength (145 \pm 9 versus 192 \pm 17 MPa, pitch versus PAN CFR PEEK,
- 12 AVG \pm SD). Fiber type did not have a significant effect on failure strain. Under cyclic loading, 13 PAN CFR PEEK demonstrated an increased resistance to FCP compared with unfilled and pitch
- 14 CFR PEEK, and this improvement was enhanced following annealing. Pitch CFR PEEK
- 14 CFR FEEK, and this improvement was enhanced following ameaning. Fich CFR FEEK 15 exhibited similar FCP behavior to unfilled PEEK and neither material was substantially affected
- 16 by annealing. The improvements in monotonic and FCP behavior of PAN CFR PEEK is
- attributed to a compound effect of inherent fiber properties, increased fiber number for an
- 17 autobuted to a compound effect of innerent noer properties, increased noer number for an 18 equivalent wt % reinforcement, and fiber aspect ratio. FCP was shown to proceed via cyclic
- 19 modes during stable crack growth, which transitioned to static modes (more akin to monotonic
- fracture) at longer crack lengths. The mechanisms of fatigue crack propagation appear similar
- 21 between carbon-fiber types.

22 1. Introduction

Poly(ether-ether-ketone) (PEEK) is a high-performance, biocompatible polymer which
has been used in load-bearing orthopedic components since the 1990s [1]. The ability to
formulate PEEK with fillers such as carbon fiber can result in mechanical properties suitable to a
variety of orthopedic applications, including spinal fusion cages, fracture fixation plates, femoral
stems, bone screws, intramedullary nails, and other devices [2].

28 The mechanical and thermal properties of PEEK are a function of its crystalline structure, 29 chemical architecture, and morphology. PEEK is a semi-crystalline thermoplastic which, 30 depending on processing, can be can be up to 43% crystalline [3], although 30-35% crystallinity is typical for PEEK used in medical devices [1,4,5]. The crystalline domains are generally 31 32 lamellar in structure and can organize into spherulites [3,6]. Crystallinity can be controlled by 33 altering the rate of cooling from the molten state during processing, or by using a post-processing 34 thermal treatment such as annealing. Since molecular chains need time and energy to organize 35 into crystalline domains, both slow cooling from the molten state and annealing enhance crystallinity in PEEK. Fillers such as carbon fiber also affect morphology by altering the 36 geometry of crystalline domains as well as local cooling rates of the PEEK matrix [4,7-9]. 37 38 The chemical backbone of PEEK is comprised of aromatic (benzene) units connected by 39 ketone and ether groups. The monomer units form a linear homopolymer with approximately 40 100 units per chain and an average molecular weight of 80,000-120,000 g/mol [1]. While the 41 molecule can rotate about the ether and ketone bonds, the large aromatic units inhibit chain mobility and require large amounts of thermal energy for bulk motion [1,4]. Accordingly, PEEK 42 43 has a high glass transition temperature (145°C), a high melting temperature (340°C) [6] and is

44 stable at the body's operating temperature of 37° C.

45	In addition to its thermal and mechanical properties, PEEK's radiolucency and radiative		
46	stability contribute to its orthopedic relevance. Metallic implants are radiopaque, inhibiting		
47	radiographic assessment of intra-implant bone formation by causing artefacts that can hinder		
48	clinical evaluation [10,11]. PEEK is radiolucent, enabling radiographic assessment using		
49	existing diagnostic imaging techniques [2]. In the spine, for example, radiographic evidence of		
50	bone density changes within a PEEK fusion cage can be used to assess the degree of fusion [12].		
51	PEEK is stable when exposed to gamma radiation in doses relevant to implant sterilization (25-		
52	40 kGy) [2], and can also be sterilized using steam and ethylene oxide without appreciable		
53	degradation in mechanical properties [13].		
54	The predominant clinical use of PEEK is in interbody fusion cages in the spine, where it		
55	is used in approximately 65% of the spinal fusion devices implanted annually in the U.S. [14].		
56	PEEK has also shown promise in fracture fixation plates [15,16] and femoral stems [17,18].		
57	Stress shielding in metallic fracture fixation plates [19] and hip stems [20] has motivated		
58	research into alternative structural materials, including PEEK. The use of carbon fiber to create		
59	a reinforced PEEK composite enables the modulus of some PEEK formulations to approximate,		
60	for example, cortical bone (approximately 17 GPa [21]), thereby theoretically reducing stress		
61	shielding. A number of carbon-fiber-reinforced (CFR) PEEK fracture fixation devices are now		
62	available and have shown promising clinical results [15,16]. PEEK as a femoral stem material		
63	has been the subject of much research and promising medium-term clinical results [22] but		
64	limited adoption in the U.S. While PEEK is used in only a fraction of the fracture fixation plates		
65	and hip stems implanted annually, its use is expected to rise with continued research and longer-		
66	term clinical data. This is especially relevant given the ongoing challenges with tissue modulus		
67	matching in orthopedic metals and the propensity for corrosion in metallic devices.		

Unfilled and CFR PEEK have also been explored as bearing surfaces for total joint
arthroplasty. *In vitro* tribological studies comparing the wear behavior of ultra-high-molecularweight polyethylene (UHMWPE) with unfilled and CFR PEEK have shown mixed results [23–
25]. Improvements in UHMWPE wear behavior, mixed PEEK data, and historical failures of
CFR polymer bearing surfaces dating back to the 1970s may limit PEEK's use as a bearing
material in the near-term. Nonetheless, new PEEK formulations are being developed and
marketed as bearing surface alternatives [26].

CFR PEEK used in orthopedics commonly utilize one of two carbon-fiber types: PAN-75 76 based carbon fibers or pitch-based carbon fibers. PAN-based carbon fibers are derived from 77 polyacrylonitrile and predominantly contain acrylonitrile monomer units, whereas pitch-based 78 carbon fibers are typically derived from petroleum products and contain thousands of aromatic 79 hydrocarbons [27,28]. The differences in carbon-fiber precursor requires different processing conditions and results in different fiber geometric and mechanical properties [27]. PAN-based 80 81 carbon fibers can be stiffer, stronger, and are typically thinner than pitch-based carbon fibers 82 (fiber elastic modulus 540 versus 280 GPa, fiber diameter 6 - 8 versus 10 - 20 µm, PAN versus pitch) [27,29,30]. The smaller diameter of PAN- compared to pitch-based carbon fibers as well 83 84 as fiber density differences can result in more numerous fibers within a PAN CFR PEEK 85 composite compared to a pitch CFR PEEK composite for an equivalent wt % reinforcement. 86 Accordingly, PAN CFR PEEK composites can be stiffer and stronger than pitch-based 87 counterparts [29]. Tribologically, PAN and pitch CFR PEEK exhibit similar wear rates, though these rates are sensitive to ambient temperature [27], dry versus lubricated articulation [25], 88 89 conformity of contact [23], among other variables. Although tribological properties appear 90 largely similar, pitch CFR PEEK is marketed as a material with beneficial tribological properties

91 (tradename PEEK-OPTIMA Wear PerformanceTM) [26].

92 While not common, in vivo fractures of PEEK implants have been documented in the literature [31,32]. Additionally, in vivo fractures of other orthopedic devices comprising 93 94 polymers (namely UHMWPE) and metals (namely cobalt-chromium, titanium, and stainless 95 steel), have been documented extensively [33–35] and remain a limiting factor in clinical 96 longevity. Despite the low prevalence of PEEK fractures, continually evolving material 97 formulations and component designs warrant an understanding of the monotonic and fatigue fracture behavior of unfilled and pitch and PAN CFR PEEK. 98 99 A number of studies have explored effects of microstructural and processing variables on 100 the fatigue and fracture behavior of PEEK [36–44]. In both unfilled and reinforced PEEK, 101 matrix molecular weight can strongly influence fatigue crack propagation (FCP) resistance and 102 the mechanisms of crack propagation [36,37,42]. An increase in molecular weight has been 103 shown to improve resistance to FCP, an effect which has been partially attributed to an increased 104 density of tie molecules connecting lamellar regions in higher molecular weight formulations, 105 thereby strengthening the polymer matrix [36,37]. In unfilled PEEK, it has been shown that 106 matrix molecular weight can precipitate differences in spherulite size, whereby spherulites will 107 tend to grow larger in lower molecular weight PEEK [42]. Subsequently, crack growth tends to 108 be intraspherulitic in lower molecular weight PEEK (i.e. through larger spherulites) and interspherulitic in higher molecular weight PEEK (i.e. around smaller spherulites) [42], 109 110 reflecting fundamentally different mechanisms of crack propagation as a function of molecular weight. Enhanced crystallinity, which can be achieved via annealing [36,41,45], has also been 111 112 shown to enhance resistance to FCP, though to a much lesser extent than molecular weight 113 [36,37]. The mechanisms driving this improvement in FCP resistance are attributed to increased

114 energy required to deform and crack organized crystalline domains compared with amorphous 115 domains [36,37]. Interestingly, while annealing increases the degree of crystallinity in unfilled 116 and reinforced PEEK by similar amounts, improvements in FCP resistance induced by annealing 117 have been shown to be greater in reinforced PEEK compared with unfilled PEEK [36]. It has 118 been suggested that strong carbon fiber/PEEK matrix bonding produces crack initiation close to 119 but not at the fiber/matrix interface (small amounts of matrix material may remain attached to the 120 fibers), and thus FCP in short CFR PEEK is strongly dependent or even dominated by matrix 121 properties, such as crystallinity, in regions close to the fibers [36]. The importance of the matrix 122 properties in FCP in short CFR PEEK is supported by saturating improvements in FCP resistance 123 with increasing fiber volume fraction [44]. While the addition of carbon fibers to a PEEK matrix 124 introduces new energy dissipation mechanisms via fiber fracture and pullout, it also constrains 125 the ability of the matrix to dissipate energy via plastic deformation [44]. Fiber fractions of 30%wt appear to offer little improvement in FCP resistance compared to volume fractions of 20% wt 126 127 due to these competing energy dissipation mechanisms [44], thus underscoring the importance of 128 matrix plasticity in FCP.

129 While previous studies have elucidated some microstructural and processing variables on 130 the fatigue and fracture behavior of PEEK, there have been no studies directly comparing the FCP behavior of PAN versus pitch CFR PEEK. In light of documented in vivo fractures of 131 132 orthopedic implants made of both polymeric and metallic components coupled with PAN and 133 pitch CFR PEEK formulations designed specifically for orthopedic applications, it is the aim of the present investigation to describe the monotonic and FCP behavior of unfilled PEEK and pitch 134 135 and PAN CFR PEEK. Additionally, the effect of annealing on FCP behavior is investigated. 136 The materials studied were formulated specifically for use in orthopedic implants.

137 2. Methods

138 2.1 Material formulations

139 Three PEEK material formulations were studied:

140 (1) Unfilled PEEK (density 1.3 g/cm³, tradename PEEK-OPTIMATM LT1, Invibio,

141 Lankashire, UK)

142 (2) PAN CFR PEEK (density 1.3 g/cm³, PEEK-OPTIMATM LT1 matrix with 30% wt

- 143 PAN carbon fibers, tradename PEEK-OPTIMA ReinforedTM, Invibio, Lankashire, UK).
- 144 Fibers are short and randomly distributed (fiber modulus 540 GPa, fiber diameter 6 ± 2

145 μ m, fiber length 230 ± 23 μ m, fiber density 1.8 g/cm³ [45])

146 (3) Pitch CFR PEEK (density 1.4 g/cm³, PEEK-OPTIMATM LT1 matrix with 30% wt

147 Pitch carbon fibers, tradename PEEK-OPTIMA Wear PerformanceTM, Invibio,

148 Lankashire, UK). Fibers are short and randomly distributed (fiber modulus 280 GPa,

fiber diameter $10 \pm 2 \mu m$, fiber length $230 \pm 13 \mu m$, fiber density 2.0 g/cm³ [45])

150 Material granules were obtained from Invibio and processed into dog-bone and compact-

tension (CT) specimens (Figure 1). Granules were first pre-heated to 70°C to remove residual

152 moisture then injection molded into plates (250 x 25 x 2.5 mm). The injection nozzle

temperature was held constant at 400°C and the mold at 250°C. Samples were cooled in air at

154 room temperature. Water-jet machining was used to cut dog-bone and CT specimens from the

155 plates, with the samples oriented for load application parallel to the mold-fill direction.

Three heat treatments were examined to investigate the effects of post-processing thermal treatment on FCP behavior. Samples were either non-annealed, annealed at 200°C, or annealed at 300°C. Annealing was conducted for five hours in a Nabertherm oven (Lilienthal, Germany),

161 2.2 Monotonic testing

Tensile testing to failure was performed on non-heat-treated samples in accordance with 162 163 ASTM D638 on type V dog-bone specimens (n=4 samples tested per material for a total of 12 164 tests). Monotonic mechanical testing for equivalent heat-treated materials has been reported elsewhere [25,46] and was therefore not repeated here. Displacement was applied at a rate of 0.5 165 166 mm/min in ambient conditions (21°C / 28% RH) using a screw-driven Instron (model 5500R). 167 Strain was measured using a video extensometer (Instron, model 2663-821). Temperature of the 168 gauge-section was not measured during monotonic testing. Due the viscoelastic nature of 169 thermoplastic polymers, reported mechanical properties should be understood within the context 170 of displacement rate and ambient temperature. However, it has been previously shown that at 171 room temperature (≈ 124 °C below PEEK's glass transition temperature), varying displacement 172 rate by over four orders of magnitude (from 0.05 to 50 mm/min) had little effect on elastic 173 modulus and increased yield stress by less than 1.4x [47].

174 Elastic modulus (E), ultimate tensile strength (σ_{ut}), and elongation at failure (ε_f) were 175 reported for each material. Elastic modulus was calculated using a secant approximation 176 between 0.1% and 0.5% strain for each specimen. Student's t-tests were used to compare E, σ_{ut} , 177 and ε_f between material formulations with significance assumed at p \leq 0.05.

178 2.3 Fatigue testing

Fatigue crack propagation (FCP) experiments were conducted on CT specimens using a
servo-hydraulic Instron (model 8871) and a load-controlled sinusoidal wave function at a
frequency of 5 Hz [41,43]. Testing was performed at room-temperature and an air-cooling

182 system was used to minimize hysteretic heating [48]. The load ratio (minimum load/maximum 183 load) was held constant at 0.1. A pre-crack of 1 mm was introduced at the tip of each notch using a razor blade and custom fixture, and datum dots were placed on specimen sides for 184 185 subsequent image analysis [48]. Crack length was measured using a variable magnification 186 optical system (Infinivar CFM-2/S, 5µm/pixel) and a digital video camera (Sony XCD-SX910). 187 A custom LabView program controlled the camera, which captured images every 500 or 1000 188 cycles, depending on crack velocity. Custom scripts were created in ImageJ and MATLAB to semi-automate data analysis. A minimum of three samples were tested for each material 189 190 formulation. The Paris equation (Equation 1) was used to map FCP as a function of cyclic stress 191 intensity, where da/dN is the rate of crack velocity (mm/cycle), ΔK is the cyclic stress intensity (i.e. the crack driving force, MPa \sqrt{m}), and C (pre-exponent) and m (exponent, slope on 192 193 logarithmic scale) are material constants. Any data not meeting the condition of small scale 194 yielding (Equation 2) were excluded from this analysis, where (W-a) is the uncracked ligament length, K_{max} is the maximum mode-one stress intensity (MPa \sqrt{m}), and σ_{ys} is the material yield 195 196 strength (MPa).

197 197 $\frac{da}{dN} = C\Delta K^m$ Equation 1 198 $(W-a) \ge \frac{4}{\pi} \left(\frac{K_{max}}{\sigma_{VS}}\right)^2$ Equation 2

199 2.4 Fractography

Fracture surfaces were imaged with scanning electron microscopy (SEM, Quanta FEI and
Versa 3D Dual Beam) at 50-500x and optical microscopy (Keyence VHX 6000) at 10-50x.
Some specimens were sputter coated in gold-vanadium to facilitate fracture surface visualization.

3. Results

204 3.1 Monotonic testing results

205 Compared with pitch CFR PEEK, PAN CFR PEEK exhibited a significantly higher 206 elastic modulus (18.5 ± 1.3 vs 12.5 ± 1.3 GPa, PAN vs pitch CFR PEEK, p = 0.006, AVG \pm SD) 207 and ultimate tensile strength (192 ± 17 vs 145 ± 9 MPa, PAN vs pitch CFR PEEK, p = 0.005, 208 AVG \pm SD) (Table 1). Strain at failure was not significantly different between fiber types (1.9 \pm 209 0.2 vs 2.2 ± 0.2 % strain, PAN vs pitch CFR PEEK, p = 0.116, AVG \pm SD) (Table 1). Unfilled 210 PEEK had a significantly lower elastic modulus $(3.9 \pm 0.2 \text{ GPa}, \text{AVG} \pm \text{SD})$ and ultimate tensile 211 strength (93 \pm 1 MPa), and a significantly higher strain at failure (66 \pm 7 %, AVG \pm SD) 212 compared with either fiber type ($p \le 0.002$) (Table 1). In terms of the stress-strain behavior, 213 unfilled PEEK demonstrated appreciable post-yield deformation (necking), whereas both pitch 214 and PAN CFR PEEK failed in a predominantly brittle manner, at low failure strains and with 215 little post-yield deformation (Figure 2).

216 *3.2 Fatigue testing results*

217 The crack velocity (da/dN) versus cyclic stress intensity (ΔK) curves for all PEEK 218 materials generally followed a linear relationship in log-log space as described by the Paris Law 219 (Equation 1, Figure 3). The region of stable crack growth was measured as $3.2 \le \Delta K \le 7.1$ MPa \sqrt{m} for unfilled PEEK, $4.2 \le \Delta K \le 6.8$ MPa \sqrt{m} for pitch CFR PEEK, and $4.6 \le \Delta K \le 8.6$ 220 221 MPa \sqrt{m} for PAN CFR PEEK (all heat treatments). A rightward shift was observed in the PAN 222 CFR PEEK data compared with the pitch CFR and unfilled PEEK data (all heat treatments). 223 This rightward shift suggests an improvement in FCP resistance—a larger cyclic stress intensity 224 was required to propagate a crack at a given velocity. The effect of annealing on FCP behavior 225 appears small for unfilled and pitch CFR PEEK, evidenced by largely overlapping da/dN versus ΔK data (Figure 3). Annealing at 300 °C appears to have a more pronounced effect for PAN 226

227 CFR PEEK, evidenced by the distinct da/dN versus ΔK data between PAN and PAN 300 (Figure
228 3).

229	To clarify and quantify these observations, least squares regression analysis was used to
230	generate best fit lines of the data (Figure 4). ΔK values at a constant crack velocity of da/dN = 2
231	\times 10 ⁻⁴ mm/cycle were compared in order to quantify the relative resistance to FCP as well as the
232	effect of annealing at an intermediate crack velocity (Table 2). The value of da/dN = 2×10^{-4}
233	mm/cycle was chosen because it represents a crack velocity approximately centered within the
234	linear (Paris) growth regime, approximately halfway between near-threshold and near fast-
235	fracture regions based on the spread of the measured data (Figure 3, Figure 4). For non-annealed
236	formulations, propagating a crack at da/dN = 2 \times 10 ⁻⁴ mm/cycle required Δ K =4.9 MPa \sqrt{m} for
237	unfilled PEEK, $\Delta K = 4.7$ MPa \sqrt{m} for pitch CFR PEEK, and $\Delta K = 5.7$ MPa \sqrt{m} for PAN CFR
238	PEEK (Table 2). Thus, non-annealed unfilled and pitch CFR PEEK require a similar ΔK for
239	intermediate crack velocities while non-annealed PAN CFR PEEK requires an increased ΔK on
240	the order of 17-21% compared with unfilled and pitch CFR PEEK, respectively. For
241	formulations annealed at 300 °C, the ΔK values required to propagate a crack at da/dN = 2 × 10 ⁻
242	4 mm/cycle remain similar between unfilled and pitch CFR PEEK (4.7 versus 4.8 MPa \sqrt{m} ,
243	respectively) but increased to 7.0 MPa \sqrt{m} for PAN CFR PEEK, representing an increase of 45-
244	50%.
245	The effect of heat-treatment on FCP resistance was thus relatively minor for unfilled
246	PEEK, with a maximum ΔK variation of 0.3 MPa \sqrt{m} (6%) amongst heat treatments at da/dN = 2

 $\times 10^{-4}$ mm/cycle. Similarly, the effect of heat treatment was relatively minor for pitch CFR

248 PEEK, with a maximum ΔK variation of 0.5 MPa \sqrt{m} (9%) amongst heat treatments at da/dN = 2

 $\times 10^{-4}$ mm/cycle. Conversely, heat-treatment had a larger effect on PAN CFR PEEK, with a

250 maximum ΔK variation of 1.5 MPa \sqrt{m} (24%) amongst heat treatments at da/dN = 2 × 10⁻⁴ 251 mm/cycle.

252 The linear regression analysis also enabled calculation of the Paris exponent (m in 253 Equation 1), a material-specific parameter describing the rate of crack acceleration. Larger 254 values of m indicate larger rates of crack accelerations. Values of m ranged between 4 - 5.1 for 255 unfilled PEEK, 6.6 – 8.0 for pitch CFR PEEK, and 5.9 – 6.3 for PAN CFR PEEK (Figure 5). 256 Thus, we observe a trend towards larger values of crack acceleration for both pitch and PAN 257 CFR PEEK compared with unfilled PEEK, suggesting that the addition of carbon-fibers can 258 increase the rate of crack acceleration. Heat-treatment appeared to have a minor and non-259 constant effect on m (Figure 5). In unfilled and pitch CFR PEEK, annealing decreased m, 260 whereas for PAN CFR PEEK, annealing at 200 °C and 300 °C resulted in an increase in m of 17% and 7%, respectively (6.9 and 6.3 versus 5.9). 261

262 3.3 Fractography

Under monotonic loading, the fracture surface of unfilled PEEK displayed macroscopic plastic deformation including tearing features and a reduced cross-sectional area at the location of fracture (a result of necking) (Figure 6). The fracture surfaces of pitch and PAN CFR PEEK were similar to each other, displaying little bulk plastic deformation in comparison with unfilled PEEK (Figure 6). Pitch and PAN CFR PEEK display fiber fracture and fiber pull-out throughout the fracture surface (Figure 6).

Under fatigue loading, unfilled PEEK exhibited striation-like markings and parabolic
features in the stable growth regime (Figure 7). The parabolic features tended to grow larger at
longer crack lengths (Figure 7E). Compared with the stable growth region, the unstable growth

273 localized contraction (necking) around the crack tip (Figure 7A).

Pitch and PAN CFR PEEK present with little macroscopic deformation (Figure 8),
resulting from suppression of plastic deformation due to the presence of carbon fibers. During
stable FCP, some fiber fracture and pull-out were observed in combination with near-tip local
deformation of the matrix material (Figure 8B, 8E). During unstable FCP, these local matrix
deformation features are not observed and the fracture surfaces instead display primarily fiber
fracture and fiber pull-out (Figure 8C, 8F).
There were no observable fractographic distinctions in macroscopic (reinforcement-level)

failure mode or mechanism between heat-treatments for unfilled PEEK and pitch and PAN CFR
PEEK. Higher imaging magnifications may illuminate crystalline-level mechanisms and
warrants further investigation.

284 4. Discussion

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It was the aim of the current study was to investigate the effects of PAN- and pitch-based

286 carbon fibers on the monotonic properties and FCP resistance of orthopedic grade PEEK.

Additionally, we sought to elucidate the effects of annealing on FCP resistance.

288 Complete crystallinity data for the materials used in this study have been reported

elsewhere [25]. Briefly, crystallinity for non-annealed PEEK is $\approx 32\%$, and all non-annealed

formulations (i.e. unfilled, pitch and PAN CFR PEEK) are within 1% of this value [25].

291 Annealing enhances crystallinity in unfilled and pitch and PAN CFR PEEK by similar amounts:

292 Low temperature (200 °C) annealing enhances crystallinity by $\approx 1\%$ while high temperature (300

293 °C) annealing enhances crystallinity by $\approx 9\%$ [25].

294 The addition of both pitch and PAN carbon fibers to the PEEK matrix increased 295 monotonic stiffness and strength and decreased ductility (strain to failure) compared with 296 unfilled PEEK. These trends are consistent with data published by the material manufacturer 297 [26,49,50] and with the behavior of many short-fiber thermoplastic polymer composites. 298 Comparing fiber types, we observed statistically significant increases of 48% in elastic modulus 299 and 32% in ultimate tensile strength, and a non-statistically significant decrease of 14% in strain 300 to failure for PAN versus pitch CFR PEEK. Increases in elastic modulus and ultimate tensile are 301 attributed to a number of microstructural characteristics, including inherent fiber mechanical 302 properties, differences in fiber number, and differences in fiber aspect ratio. The PAN-based 303 carbon fibers used in this study are 93% stiffer than pitch-based carbon fibers (elastic modulus 304 540 versus 280 GPa, PAN- versus pitch-based carbon fibers, respectively) [29]. Thus, composite 305 mechanical property differences would be expected even if other parameters (fiber number, fiber 306 aspect ratio, interfacial bonding, crystallinity, etc.) were equivalent. Further, PAN-based carbon 307 fibers are thinner and less dense than pitch-based carbon fibers (diameter 6 versus 10 μ m, density 1.8 versus 2.0 g/cm³, PAN- versus pitch-based carbon fibers, respectively), and we thus 308 309 expect ≈3.1 times more PAN-based carbon fibers in a given specimen compared with pitch-310 based carbon fibers for an equivalent wt % reinforcement (both composites used in this study 311 contained 30% wt fiber reinforcement). In a related vein, since the diameter of PAN-based 312 carbon fibers are smaller than pitch-based carbon fibers, the ratio of fiber surface area to fiber 313 volume will be enhanced in PAN versus pitch CFR PEEK for an equivalent fiber volume 314 fraction, thereby providing more surface area for the PEEK matrix to bond to PAN-based carbon 315 fibers. We suggest that improvements in mechanical behavior for PAN versus pitch CFR PEEK 316 are attributed to these compound effects: PAN-based carbon fibers are themselves stiffer, more

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area is exposed to PEEK matrix, thus enhancing the area available for fiber/matrix bonding.

PAN-based carbon fibers are present, and comparatively more PAN-based carbon fiber surface

Under fatigue loading, we found that the addition of pitch-based carbon fibers did not
enhance FCP resistance, as the da/dN versus ΔK behavior for unfilled and pitch CFR PEEK are
similar. FCP resistance of these materials was largely unaffected by either low-temperature (200
°C) or high-temperature (300 °C) annealing. Conversely, the FCP resistance of PAN CFR PEEK
was appreciably improved compared with unfilled and pitch CFR PEEK. For non and lowtemperature annealed PAN CFR PEEK, the improvement was on the order of 17-21%, while for
high-temperature annealed PAN CFR PEEK the improvement was on the order of 45-50% at an
intermediate crack velocity.

The complex interdependence of microstructural parameters including manufacturingand annealing-induced matrix crystallinity, fiber type, fiber number, and fiber aspect ratio, coupled with complex dynamics of FCP in polymer composites, make it difficult to unambiguously differentiate individual microstructural effects on FCP behavior. Yet, a number of observations warrant discussion.

332 The addition of fibers to a polymer matrix can enhance resistance to FCP by introducing 333 energy dissipation mechanisms via fiber fracture and pull-out [44]. Simultaneously, fibers can 334 inhibit energy dissipation by limiting the ability of the matrix to deform plastically [44]. The 335 balance between net energy dissipation/absorption (thus FCP improvement/degradation) depends 336 on a balance between matrix ductility (which depends on matrix molecular weight, crystallinity, 337 etc.), fiber properties, and the properties of the fiber/matrix interface. Previous studies have 338 shown that the addition of 30% wt. randomly distributed short glass fibers to a PEEK matrix 339 provided little to no improvement in FCP resistance, while the addition of 30% wt. randomly

340 distributed carbon fibers provided at least some improvement in FCP resistance [36,41,43] (the 341 carbon fiber type is not mentioned in these studies, however PAN-based carbon fibers are the 342 likely historical precedent [51]). This phenomenon is attributed to stronger fiber/matrix adhesion 343 between the carbon fibers and the PEEK matrix compared with glass fibers and the PEEK matrix 344 [36,41,44]. The results found in the current study, in which the addition of pitch-based carbon 345 fibers provided little to no improvement in FCP resistance, while the addition of PAN-based 346 carbon fibers provided an appreciable improvement in FCP resistance, could be plausibly 347 explained via the same mechanism; stronger fiber/matrix adhesion in PAN- compared with pitch-348 based PEEK composites. However, aforementioned differences in inherent fiber properties, fiber 349 numbers, and fiber aspect ratios confound and preclude a definitive statement on interfacial bond 350 strength. Indeed, the fact that observed improvements in FCP resistance for PAN CFR PEEK 351 are not commensurate with the magnitude of differences in fiber properties or fiber number could 352 plausibly suggest a weaker interfacial bond for PAN versus pitch CFR PEEK. Additional studies 353 are required to clarify differences in interfacial bond strength, which could be achieved via FCP 354 tests controlling for fiber aspect ratio and/or fiber number.

355 Annealing has been shown to have a greater impact on FCP resistance for CFR PEEK 356 compared with unfilled PEEK (carbon fiber type not specified), even when similar overall 357 increases in crystallinity are induced by annealing [36,41]. Results found in the current study for 358 PAN CFR PEEK are similar—annealing had no measurable effect on unfilled PEEK but 359 appreciably improved FCP resistance in PAN CFR PEEK. It has been suggested that annealing 360 may preferentially influence the matrix in regions near the fiber/matrix interface [36]. Thus, 361 while it is not clear why annealing had no measurable effect on pitch CFR PEEK, one plausible 362 explanation is that a lower fiber number in pitch versus PAN CFR PEEK (thus fewer

fiber/matrix interfacial regions) makes any preferential improvements in crystallinity less
pronounced. It has also been suggested that annealing enhances crystalline growth of the PEEK
matrix onto the carbon fiber surface, thereby improving interfacial bond strength [41]. Thus, a
second and related explanation follows that differences in crystallization mechanisms between
PAN and pitch CFR PEEK [45] contribute to differences in interfacial bond strength as a
function of annealing, even for similar overall degrees of crystallinity.

Fractographic analysis of failure surfaces suggest two distinct modes of FCP in PEEK,
notably a cyclic mode acting at low crack growth rates and a static mode acting at high crack
growth rates, as described by previous studies [37,38,40,43,44].

372 In unfilled PEEK, the stable growth regime exhibited striation-like markings (Figure 7B, 373 7C), similar to those reported previously [37,38,40,41,44], presumably caused by crack blunting 374 and re-sharpening during cyclic loading. The average width of the striation-like bands were not 375 measured in this study and compared to da/dN to confirm whether they were true fatigue 376 striations. Yet, previous investigations [37,40,41] confirmed markings of similar size and 377 morphology to be true fatigue striations. The observed parabolic features (Figure 7C, 7E) are 378 also consistent with previous investigations [37,41,44], and are attributed to the intersection of 379 the primary crack front with secondary cracks induced by inherent flaws. Unlike the stable 380 growth regime, the fast-fracture regime in unfilled PEEK is characterized by ductile contraction 381 (i.e. necking) in the zone around the crack tip. This ductile contraction in fast fracture region is 382 not apparent during stable crack growth but is apparent for monotonically tested PEEK.

Failure surfaces of pitch and PAN CFR PEEK also show evidence of an interaction
between cyclic and static mechanisms during FCP in line with previous studies on CFR PEEK
[44]. At low crack growth rates, we observe regions of matrix deformation and rupture near to

386 and along the fiber/matrix interface, as well as fiber fracture and pull-out (Figure 8B, 8E). It has 387 been previously shown that under cyclic loading, local failure is dominated by separation along 388 the fiber/matrix interfaces and rupture of the matrix material between fibers [36,43]. At higher 389 crack growth rates, equivalent matrix deformation is not observed, and the fracture surface is 390 instead comprised primarily of fiber fracture and pull-out (Figure 8C, 8F) more akin to 391 monotonically tested samples (Figure 6). Thus, our findings offer supporting evidence for cyclic 392 modes of growth at low growth rates which transition to static modes near the onset of failure in unfilled and both pitch and PAN CFR PEEK. 393

394 While the CFR PEEK formulations used in this study were reinforced using short, 395 randomly distributed fibers to achieve bulk isotropy, the injection molding process has been 396 shown to introduce some fiber alignment in proximity to the specimen surface (i.e. a "skin" 397 layer) induced by friction with the mold wall [29,36,41,43,44]. This well-documented skin-core 398 structure has been shown to produce more rapid crack growth when load is applied perpendicular 399 to the mold-fill direction (thus crack growth parallel to the mold-fill direction) compared with the 400 converse orientation [43,44]. Thus, the results here are limited to load application parallel to the mold fill direction. 401

402 **5.** Conclusion

Under monotonic loading, PAN CFR PEEK exhibited a larger elastic modulus and
ultimate tensile strength compared with unfilled and pitch CFR PEEK. Under cyclic loading,
PAN CFR PEEK exhibited an improved resistance to fatigue crack propagation compared with
unfilled and pitch CFR PEEK. The improvement in fatigue crack propagation resistance for
PAN CFR PEEK was enhanced following high-temperature (300 °C) annealing.

408 Pitch CFR PEEK did not exhibit improved fatigue crack propagation resistance compared 409 with unfilled PEEK. Neither low temperature (200 °C) nor high temperature (300 °C) annealing 410 produced a measurable effect on the fatigue crack propagation behavior of these materials. 411 The improvement in mechanical properties for PAN CFR PEEK is attributed to a 412 compound affect: PAN-based carbon fibers are themselves stiffer than pitch-based carbon fibers, 413 more PAN-based carbon fibers are present compared with pitch-based carbon fibers for an equivalent wt % reinforcement, and comparatively more PAN-based carbon fiber surface area is 414 415 exposed to PEEK matrix, thus enhancing the area available for fiber/matrix bonding. 416 Differences in fiber/matrix interfacial bond strength between PAN- versus pitch-based carbon 417 fibers should be further elucidated, possibly via studies controlling for fiber number and/or 418 aspect ratio. 419 Fatigue crack propagation was shown to proceed via cyclic modes during stable crack 420 growth, characterized by striation-like bands and parabolic features in unfilled PEEK and matrix 421 rupture near to and along the fiber/matrix interface in pitch and PAN CFR PEEK. Cyclic modes 422 transition to static modes (more akin to monotonic fracture) at longer crack lengths, 423 characterized by necking in unfilled PEEK and an increased degree of fiber fracture and pull-out 424 in pitch and PAN CFR PEEK. The mechanisms of fatigue crack propagation appear similar 425 between carbon-fiber types.

6. Figures and Tables



Figure 1. A) ASTM D638 type V dog-bone specimens used for monotonic testing. B) Compacttension (CT) specimen used for FCP testing. C) Thickness for all specimens. Samples were oriented for load application parallel to the mold fill direction. Drawings are not to scale.

Table 1. Material properties for PEEK materials (non-heat-
treated formulations).

	Unfilled	Pitch	PAN
E (GPa)	3.9 ± 0.2	12.5 ± 1.3	18.5 ± 2.3
σ_{ut} (MPa)	93 ± 1	145 ± 9	192 ± 17
ε _f (%)	66 ± 7	2.2 ± 0.2	1.9 ± 0.2



Figure 2. Representative stress-strain plots for Pitch CFR PEEK, PAN CFR PEEK, and unfilled PEEK (non heat-treated formulations).



445 Figure 3. FCP plots for all material formulations and heat-treatments.



Figure 4. Paris fits for all materials. A constant crack velocity of $da/dN = 2 \times 10^{-4}$ mm/cycle was chosen to represent an intermediate crack velocity.

469	materials.
467	velocity of $da/dN = 2 \times 10^{-4}$ mm/cycle for all
167	Table 2 AK values at the intermediate grack

	ΔK (MPa√m) at da/dN = 2 × 10 ⁻⁴ mm/cycle
Unfilled	
0°C	4.9
200 °C	5.0
300 °C	4.7
Pitch	
0°C	4.7
200 °C	4.3
300 °C	4.8
PAN	
0°C	5.7
200 °C	5.6
300 °C	7.0







478 Figure 6. SEM images of the fracture surfaces of monotonically tested samples (non-heat-treated formulations).



- 481 Figure 7. Images of the fracture surfaces of fatigue tested unfilled PEEK (non-heat-treated
- formulations). B: Early growth region. C: Mid growth region. D: Fast fracture region. E: Mid-
- to-late growth region.



- 485 Figure 8. Images of the fracture surfaces of fatigue tested pitch (top) and PAN (bottom) CFR
- PEEK (non-heat-treated formulations). B and E: Early growth region. C and F: Fast fracture region.

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492 8. Bibliography

- 493 [1] Kurtz S. An Overview of PEEK Biomaterials. In: Kurtz S, editor. PEEK Biomaterials
 494 Handbook. 2012. p. 1–7.
- 495 [2] Kurtz S, Devine J. PEEK biomaterials in trauma, orthopedic, and spinal implants.
 496 *Biomaterials*. 2007;28(32):4845–69.
- 497 [3] Kumar S, Anderson D, Adams W. Crystallization and Morphology of Poly(aryl-ether498 ether-ketone). *Polymer (Guildf)*. 1986;27:329–36.
- 499 [4] Reitman M, Jaekel D, Siskey R, et al. Morphology and crystalline architecture of
 500 polyaryletherketones. In: Kurtz S, editor. PEEK Biomaterials Handbook. 2012. p. 49–60.
- 501 [5] Green S, Schlegel J. A Polyaryletherketone Biomaterial for use in Medical Implant
 502 Applications. In: Polymers for the Medical Industry, Proceedings of a Conference held in
 503 Brussels. 2001. p. 1–7.
- 504 [6] Blundell D, Osborn B. The Morphology of Poly(aryl-ether-ether-ketone). *Polymer* 505 (*Guildf*). 1983;24:953–8.
- Tung C, Dynes P. Morphological characterization of polyetheretherketone-carbon fiber
 composites. *J Appl Polym Sci.* 1987;33:505–20.
- 508 [8] Mehmet-Alkan A, Hay J. The Crystallinity of PEEK Composites. *Polymer (Guildf)*.
 509 1993;34(16):3529–31.
- 510 [9] Velisaris C, Seferis J. Heat Transfer Effects on the Processinge-Structure Relationships of
 511 Polyetheretherketone (PEEK) Based Composites. *Polym Eng Sci.* 1988;28(9):583–91.
- 512 [10] Ernstberger T, Buchhorn G, Heidrich G. Artifacts in spine magnetic resonance imaging
 513 due to different intervertebral test spacers. *Neuroradiology*. 2008;51:525–9.
- 514 [11] Panfili E, Pierdicca L, Salvolini L, et al. Magnetic resonance imaging (MRI) artefacts in
 515 hip prostheses: A comparison of different prosthetic compositions. *Radiol Medica*.
 516 2014;119:113–20.
- 517 [12] Brantigan J, Steffee A. A Carbon Fiber Implant to Aid Interbody Lumbar Fusion: Two518 Year Clinical Results in the First 26 Patients. *Spine (Phila Pa 1976)*. 1993;18(14):2106–
 519 17.
- [13] Sastri V. High-Temperature Engineering Thermoplastics: Polysulfones, Polyimides,
 Polysulfides, Polyketones, Liquid Crystalline Polymers, and Fluoropolymers. In: Plastics
 in Medical Devices. 2nd ed. 2014. p. 173–213.
- 523 [14] Kurtz S. Applications of polyaryletheretherketone in spinal implants. In: Kurtz S, editor.
 524 PEEK Biomaterials Handbook. 2012. p. 231–51.
- 525 [15] Rotini R, Cavaciocchi M, Fabbri D, et al. Proximal Humeral Fracture Fixation:
 526 Multicenter Study with Carbon Fiber PEEK Plate. *Musculoskelet Surg.* 2015;99:1–8.
- 527 [16] Schliemann B, Hartensuer R, Koch T, et al. Treatment of Proximal Humerus Fractures
 528 with a CFR-PEEK Plate: 2-year Results of a Prospective Study and Comparison to
 529 Fixation with a Conventional Locking Plate. J Shoulder Elb Surg. 2015;1282–8.
- 530 [17] Akhavan S, Matthiesen M, Schulte L, et al. Clinical and histologic results related to a low-modulus composite total hip replacement stem. *J Bone Jt Surg.* 2006;88:1308–14.

Glassman A. Composite femoral stem for total hip arthroplasty. Curr Opin Orthop. 532 [18] 533 2008;19(1):6–10. 534 Uhthoff H, Poitras P, Backman D. Internal Plate Fixation of Fractures: Short History and [19] 535 Recent Developments. J Orthop Sci. 2006;11:118-26. 536 Bugbee W, Culpepper W, Engh C, et al. Long-Term Clinical Consequences of Stress-[20] 537 Shielding After Total Hip Arthroplasty Without Cement. J Bone Jt Surg. 1997;79(7):1007-12. 538 539 [21] Reilly D, Burstein A. The elastic and ultimate properties of compact bone tissue. J 540 Biomech. 1975;8(6). 541 Li C, Vannabouathong C, Sprague S, et al. The use of carbon-fiber-reinforced (CFR) [22] 542 PEEK material in orthopedic implants: A systematic review. Clin Med Insights Arthritis 543 Musculoskelet Disord. 2014;8:33-45. 544 Wang A, Lin R, Stark C, et al. Suitability and limitations of carbon fiber reinforced PEEK [23] composites as bearing surfaces for total joint replacements. Wear. 1999;225-229:724-7. 545 Polineni V, Wang A, Essner A, et al. Characterization of Carbon Fiber-Reinforced PEEK 546 [24] 547 Composite for use as a Bearing Material in Total Hip Replacements. ASTM Int. 1998;266-548 73. 549 [25] Regis M, Lanzutti A, Bracco P, et al. Wear behavior of medical grade PEEK and CFR 550 PEEK under dry and bovine serum conditions. Wear. 2018;408-409(May):86-95. 551 [26] Invibio. PEEK-OPTIMA Wear Performance: Typical Material Properties [Internet]. 2013 552 [cited 2016 May 2]. Available from: https://invibio.com/ortho/materials/peek-optimawear-performance 553 554 Flock J, Friedrich K, Yuan Q. On the friction and wear behaviour of PAN-and pitch-[27] carbon fiber reinforced PEEK composites. Wear. 1999;225-229:304-11. 555 Huang X. Fabrication and properties of carbon fibers. Materials (Basel). 2009;2(4):2369-556 [28] 557 403. 558 Regis M, Fusi S, Favaloro R, et al. CFR PEEK composites for orthopaedic applications. [29] 559 In: 9th International Conference on Composite Science and Technology. 2013. 560 Yuan Q, Bateman S, Friedrich K. Thermal and mechanical properties of PAN- and pitch-[30] 561 based carbon fiber reinforced PEEK composites. J Thermoplast Compos Mater. 2008;21(4):323-36. 562 563 Sardar Z, Jarzem P. Failure of a Carbon Fiber-Reinforced Polymer Implant Used for [31] 564 Transforaminal Lumbar Interbody Fusion. Glob Spine J. 2013;3(4):253-6. Tullberg T. Failure of a Carbon Fiber Implant. A Case Report. Spine (Phila Pa 1976). 565 [32] 1998;23(16):1804-6. 566 Ansari F, Chang J, Huddleston J, et al. Fractography and oxidative analysis of gamma 567 [33] inert sterilized posterior-stabilized tibial insert post fractures: Report of two cases. Knee. 568 569 2013;20(6):609-13. 570 [34] Tower A, Currier J, Currier B, et al. Rim Cracking of the Cross-Linked After Total Hip 571 Arthroplasty. J Bone Jt Surg. 2007;2212–7. Bonnheim N, Gramling H, Ries M, et al. Fatigue fracture of a cemented Omnifit CoCr 572 [35] 573 femoral stem: implant and failure analysis. Arthroplast Today. 2017;3:234-8. Saib K, Isaac D, Evans W. Effects of processing variables on fatigue in molded PEEK and 574 [36] its short fiber composites. Mater Manuf Process. 1994;9(5):829-50. 575 576 [37] Saib K, Evans W, Isaac D. The role of microstructure during fatigue crack growth in poly (aryl ether ether ketone) (PEEK). Polymer (Guildf). 1993;34(15):3198-203. 577

579 40. 580 Brillhart M, Botsis J. Fatigue fracture behavior of PEEK: 2. Effects of thickness and [39] 581 temperature. Polymer (Guildf). 1992;33(24):5225-32. Brillhart M, Gregory B, Botsis J. Fatigue fracture behavior of PEEK: 1. Effects of load 582 [40] level. Polymer (Guildf). 1991;32(9):1605-11. 583 Karger-Kocsis J, Walter R, Friedrich K. Annealing effects on the fatigue crack 584 [41] 585 propagation of injection-moulded PEEK and its short fibre composites. J Polym Eng. 586 1988;8(3-4):221-53. 587 Chu J, Schultz J. The influence of microstructure on the failure behaviour of PEEK. J [42] 588 Mater Sci. 1990;25:3746-52. 589 Friedrich K, Walter R, Voss H, et al. Effect of short fibre reinforcement on the fatigue [43] 590 crack propogation and fracture of PEEK-matrix composites. Composites. 1986;17(3):205-591 16. [44] Evans W, Isaac D, Saib K. The effect of short carbon fibre reinforcement on fatigue crack 592 593 growth in PEEK. Composites. 1996;27A:547-54. 594 Regis M, Zanetti M, Pressacco M, et al. Opposite role of different carbon fiber [45] 595 reinforcements on the non-isothermal crystallization behavior of poly(etheretherketone). 596 Mater Chem Phys. Elsevier B.V; 2016;179:223-31. 597 [46] Regis M, Bellare A, Pascolini T, et al. Characterization of thermally annealed PEEK and 598 CFR-PEEK composites. Polym Degrad Stab. 2017;136:121-30. 599 Maksimov R, Kubat J. Time and temperature dependent deformation of poly(ether ether [47] 600 ketone) (PEEK). Mech Compos Mater. 1997;33(6):517-25. 601 [48] Ansari F. The Interplay of Design and Materials in Orthopedics: Evaluating the Impact of 602 Notch Geometry on Fatigue Failure of UHMWPE Joint Replacements. Dissertation, UC Berkeley. 2015. 603 Invibio. PEEK-OPTIMA Natural: Typical Material Properties [Internet]. 2013 [cited 2016 604 [49] 605 Apr 18]. Available from: https://invibio.com/library?id=%7B9ec81b92-8ab8-40da-af8f-606 6c3bf002aa84%7D 607 Invibio. PEEK-OPTIMA Reinforced: Mechanical Properties, Physical Properties and [50] 608 Biocompatibility [Internet]. 2014 [cited 2016 Apr 18]. Available from: 609 https://invibio.com/library?id=%7B4957faed-3d7d-466b-bed0-f8dfcf1a6e5a%7D

Lafdi K, Wright M. Carbon fibers. In: Peters S, editor. Handbook of Composites. London:

Brillhart M, Botsis J. Fatigue crack growth analysis in PEEK. Int J Fatigue. 1994;16:134-

611 612

610

[51]

Chapman & Hall; 1998. p. 169–201.

578

[38]