

AperTO - Archivio Istituzionale Open Access dell'Università di Torino

## Effect of carbon fiber type on monotonic and fatigue properties of orthopedic grade PEEK

### This is the author's manuscript

*Original Citation:*

*Availability:*

This version is available <http://hdl.handle.net/2318/1688286> since 2019-01-29T11:36:26Z

*Published version:*

DOI:10.1016/j.jmbbm.2018.10.033

*Terms of use:*

Open Access

Anyone can freely access the full text of works made available as "Open Access". Works made available under a Creative Commons license can be used according to the terms and conditions of said license. Use of all other works requires consent of the right holder (author or publisher) if not exempted from copyright protection by the applicable law.

(Article begins on next page)

## **Effect of carbon fiber type on monotonic and fatigue properties of orthopedic grade PEEK**

Keywords: PEEK composites; fatigue crack propagation; orthopedic biomaterials; fractography

Noah Bonnheim, MS (corresponding author)  
Department of Mechanical Engineering, University of California, Berkeley  
2121 Etcheverry Hall  
Berkeley, CA 94720  
noah.bonnheim@berkeley.edu  
(214) 288-1730  
*No conflicts of interest*

Farzana Ansari, PhD  
Exponent, Inc.  
149 Commonwealth Drive  
Menlo Park, CA 94025  
*No conflicts of interest*

Marco Regis, PhD  
Department of Chemistry, Università degli Studi di Torino  
Via P. giuria 7  
10125 Torino Italy  
*No conflicts of interest*

Pierangiola Bracco, PhD  
Department of Chemistry, Università degli Studi di Torino  
Via P. giuria 7  
10125 Torino Italy  
*No conflicts of interest*

Lisa Pruitt, PhD  
Department of Mechanical Engineering, University of California, Berkeley  
2121 Etcheverry Hall  
Berkeley, CA 94720  
*No conflicts of interest*

**1 Abstract**

2  
3 Carbon-fiber reinforced (CFR) PEEK implants are used in orthopedic applications ranging from  
4 fracture fixation plates to spinal fusion cages. Documented implant failures and increasing  
5 volume and variety of CFR PEEK implants warrant a clearer understanding of material behavior  
6 under monotonic and cyclic loading. To address this issue, we conducted monotonic and fatigue  
7 crack propagation (FCP) experiments on orthopedic grade unfilled PEEK and two formulations  
8 of CFR PEEK (PAN- and pitch-based carbon fibers). The effect of annealing on FCP behavior  
9 was also studied. Under monotonic loading, fiber type had a statistically significant effect on  
10 elastic modulus ( $12.5 \pm 1.3$  versus  $18.5 \pm 2.3$  GPa, pitch versus PAN CFR PEEK, AVG  $\pm$  SD)  
11 and on ultimate tensile strength ( $145 \pm 9$  versus  $192 \pm 17$  MPa, pitch versus PAN CFR PEEK,  
12 AVG  $\pm$  SD). Fiber type did not have a significant effect on failure strain. Under cyclic loading,  
13 PAN CFR PEEK demonstrated an increased resistance to FCP compared with unfilled and pitch  
14 CFR PEEK, and this improvement was enhanced following annealing. Pitch CFR PEEK  
15 exhibited similar FCP behavior to unfilled PEEK and neither material was substantially affected  
16 by annealing. The improvements in monotonic and FCP behavior of PAN CFR PEEK is  
17 attributed to a compound effect of inherent fiber properties, increased fiber number for an  
18 equivalent wt % reinforcement, and fiber aspect ratio. FCP was shown to proceed via cyclic  
19 modes during stable crack growth, which transitioned to static modes (more akin to monotonic  
20 fracture) at longer crack lengths. The mechanisms of fatigue crack propagation appear similar  
21 between carbon-fiber types.

## 22 1. Introduction

23 Poly(ether-ether-ketone) (PEEK) is a high-performance, biocompatible polymer which  
24 has been used in load-bearing orthopedic components since the 1990s [1]. The ability to  
25 formulate PEEK with fillers such as carbon fiber can result in mechanical properties suitable to a  
26 variety of orthopedic applications, including spinal fusion cages, fracture fixation plates, femoral  
27 stems, bone screws, intramedullary nails, and other devices [2].

28 The mechanical and thermal properties of PEEK are a function of its crystalline structure,  
29 chemical architecture, and morphology. PEEK is a semi-crystalline thermoplastic which,  
30 depending on processing, can be up to 43% crystalline [3], although 30-35% crystallinity  
31 is typical for PEEK used in medical devices [1,4,5]. The crystalline domains are generally  
32 lamellar in structure and can organize into spherulites [3,6]. Crystallinity can be controlled by  
33 altering the rate of cooling from the molten state during processing, or by using a post-processing  
34 thermal treatment such as annealing. Since molecular chains need time and energy to organize  
35 into crystalline domains, both slow cooling from the molten state and annealing enhance  
36 crystallinity in PEEK. Fillers such as carbon fiber also affect morphology by altering the  
37 geometry of crystalline domains as well as local cooling rates of the PEEK matrix [4,7-9].

38 The chemical backbone of PEEK is comprised of aromatic (benzene) units connected by  
39 ketone and ether groups. The monomer units form a linear homopolymer with approximately  
40 100 units per chain and an average molecular weight of 80,000-120,000 g/mol [1]. While the  
41 molecule can rotate about the ether and ketone bonds, the large aromatic units inhibit chain  
42 mobility and require large amounts of thermal energy for bulk motion [1,4]. Accordingly, PEEK  
43 has a high glass transition temperature (145°C), a high melting temperature (340°C) [6] and is  
44 stable at the body's operating temperature of 37°C.

45           In addition to its thermal and mechanical properties, PEEK's radiolucency and radiative  
46 stability contribute to its orthopedic relevance. Metallic implants are radiopaque, inhibiting  
47 radiographic assessment of intra-implant bone formation by causing artefacts that can hinder  
48 clinical evaluation [10,11]. PEEK is radiolucent, enabling radiographic assessment using  
49 existing diagnostic imaging techniques [2]. In the spine, for example, radiographic evidence of  
50 bone density changes within a PEEK fusion cage can be used to assess the degree of fusion [12].  
51 PEEK is stable when exposed to gamma radiation in doses relevant to implant sterilization (25-  
52 40 kGy) [2], and can also be sterilized using steam and ethylene oxide without appreciable  
53 degradation in mechanical properties [13].

54           The predominant clinical use of PEEK is in interbody fusion cages in the spine, where it  
55 is used in approximately 65% of the spinal fusion devices implanted annually in the U.S. [14].  
56 PEEK has also shown promise in fracture fixation plates [15,16] and femoral stems [17,18].  
57 Stress shielding in metallic fracture fixation plates [19] and hip stems [20] has motivated  
58 research into alternative structural materials, including PEEK. The use of carbon fiber to create  
59 a reinforced PEEK composite enables the modulus of some PEEK formulations to approximate,  
60 for example, cortical bone (approximately 17 GPa [21]), thereby theoretically reducing stress  
61 shielding. A number of carbon-fiber-reinforced (CFR) PEEK fracture fixation devices are now  
62 available and have shown promising clinical results [15,16]. PEEK as a femoral stem material  
63 has been the subject of much research and promising medium-term clinical results [22] but  
64 limited adoption in the U.S. While PEEK is used in only a fraction of the fracture fixation plates  
65 and hip stems implanted annually, its use is expected to rise with continued research and longer-  
66 term clinical data. This is especially relevant given the ongoing challenges with tissue modulus  
67 matching in orthopedic metals and the propensity for corrosion in metallic devices.

68 Unfilled and CFR PEEK have also been explored as bearing surfaces for total joint  
69 arthroplasty. *In vitro* tribological studies comparing the wear behavior of ultra-high-molecular-  
70 weight polyethylene (UHMWPE) with unfilled and CFR PEEK have shown mixed results [23–  
71 25]. Improvements in UHMWPE wear behavior, mixed PEEK data, and historical failures of  
72 CFR polymer bearing surfaces dating back to the 1970s may limit PEEK’s use as a bearing  
73 material in the near-term. Nonetheless, new PEEK formulations are being developed and  
74 marketed as bearing surface alternatives [26].

75 CFR PEEK used in orthopedics commonly utilize one of two carbon-fiber types: PAN-  
76 based carbon fibers or pitch-based carbon fibers. PAN-based carbon fibers are derived from  
77 polyacrylonitrile and predominantly contain acrylonitrile monomer units, whereas pitch-based  
78 carbon fibers are typically derived from petroleum products and contain thousands of aromatic  
79 hydrocarbons [27,28]. The differences in carbon-fiber precursor requires different processing  
80 conditions and results in different fiber geometric and mechanical properties [27]. PAN-based  
81 carbon fibers can be stiffer, stronger, and are typically thinner than pitch-based carbon fibers  
82 (fiber elastic modulus 540 versus 280 GPa, fiber diameter 6 - 8 versus 10 - 20  $\mu\text{m}$ , PAN versus  
83 pitch) [27,29,30]. The smaller diameter of PAN- compared to pitch-based carbon fibers as well  
84 as fiber density differences can result in more numerous fibers within a PAN CFR PEEK  
85 composite compared to a pitch CFR PEEK composite for an equivalent wt % reinforcement.  
86 Accordingly, PAN CFR PEEK composites can be stiffer and stronger than pitch-based  
87 counterparts [29]. Tribologically, PAN and pitch CFR PEEK exhibit similar wear rates, though  
88 these rates are sensitive to ambient temperature [27], dry versus lubricated articulation [25],  
89 conformity of contact [23], among other variables. Although tribological properties appear  
90 largely similar, pitch CFR PEEK is marketed as a material with beneficial tribological properties

91 (tradename PEEK-OPTIMA Wear Performance<sup>TM</sup>) [26].

92           While not common, *in vivo* fractures of PEEK implants have been documented in the  
93 literature [31,32]. Additionally, *in vivo* fractures of other orthopedic devices comprising  
94 polymers (namely UHMWPE) and metals (namely cobalt-chromium, titanium, and stainless  
95 steel), have been documented extensively [33–35] and remain a limiting factor in clinical  
96 longevity. Despite the low prevalence of PEEK fractures, continually evolving material  
97 formulations and component designs warrant an understanding of the monotonic and fatigue  
98 fracture behavior of unfilled and pitch and PAN CFR PEEK.

99           A number of studies have explored effects of microstructural and processing variables on  
100 the fatigue and fracture behavior of PEEK [36–44]. In both unfilled and reinforced PEEK,  
101 matrix molecular weight can strongly influence fatigue crack propagation (FCP) resistance and  
102 the mechanisms of crack propagation [36,37,42]. An increase in molecular weight has been  
103 shown to improve resistance to FCP, an effect which has been partially attributed to an increased  
104 density of tie molecules connecting lamellar regions in higher molecular weight formulations,  
105 thereby strengthening the polymer matrix [36,37]. In unfilled PEEK, it has been shown that  
106 matrix molecular weight can precipitate differences in spherulite size, whereby spherulites will  
107 tend to grow larger in lower molecular weight PEEK [42]. Subsequently, crack growth tends to  
108 be intraspherulitic in lower molecular weight PEEK (i.e. through larger spherulites) and  
109 interspherulitic in higher molecular weight PEEK (i.e. around smaller spherulites) [42],  
110 reflecting fundamentally different mechanisms of crack propagation as a function of molecular  
111 weight. Enhanced crystallinity, which can be achieved via annealing [36,41,45], has also been  
112 shown to enhance resistance to FCP, though to a much lesser extent than molecular weight  
113 [36,37]. The mechanisms driving this improvement in FCP resistance are attributed to increased

114 energy required to deform and crack organized crystalline domains compared with amorphous  
115 domains [36,37]. Interestingly, while annealing increases the degree of crystallinity in unfilled  
116 and reinforced PEEK by similar amounts, improvements in FCP resistance induced by annealing  
117 have been shown to be greater in reinforced PEEK compared with unfilled PEEK [36]. It has  
118 been suggested that strong carbon fiber/PEEK matrix bonding produces crack initiation close to  
119 but not at the fiber/matrix interface (small amounts of matrix material may remain attached to the  
120 fibers), and thus FCP in short CFR PEEK is strongly dependent or even dominated by matrix  
121 properties, such as crystallinity, in regions close to the fibers [36]. The importance of the matrix  
122 properties in FCP in short CFR PEEK is supported by saturating improvements in FCP resistance  
123 with increasing fiber volume fraction [44]. While the addition of carbon fibers to a PEEK matrix  
124 introduces new energy dissipation mechanisms via fiber fracture and pullout, it also constrains  
125 the ability of the matrix to dissipate energy via plastic deformation [44]. Fiber fractions of 30%  
126 wt appear to offer little improvement in FCP resistance compared to volume fractions of 20% wt  
127 due to these competing energy dissipation mechanisms [44], thus underscoring the importance of  
128 matrix plasticity in FCP.

129         While previous studies have elucidated some microstructural and processing variables on  
130 the fatigue and fracture behavior of PEEK, there have been no studies directly comparing the  
131 FCP behavior of PAN versus pitch CFR PEEK. In light of documented *in vivo* fractures of  
132 orthopedic implants made of both polymeric and metallic components coupled with PAN and  
133 pitch CFR PEEK formulations designed specifically for orthopedic applications, it is the aim of  
134 the present investigation to describe the monotonic and FCP behavior of unfilled PEEK and pitch  
135 and PAN CFR PEEK. Additionally, the effect of annealing on FCP behavior is investigated.  
136 The materials studied were formulated specifically for use in orthopedic implants.

## 137 2. Methods

### 138 2.1 Material formulations

139 Three PEEK material formulations were studied:

140 (1) Unfilled PEEK (density 1.3 g/cm<sup>3</sup>, tradename PEEK-OPTIMA™ LT1, Invibio,  
141 Lankashire, UK)

142 (2) PAN CFR PEEK (density 1.3 g/cm<sup>3</sup>, PEEK-OPTIMA™ LT1 matrix with 30% wt  
143 PAN carbon fibers, tradename PEEK-OPTIMA Reinforced™, Invibio, Lankashire, UK).  
144 Fibers are short and randomly distributed (fiber modulus 540 GPa, fiber diameter 6 ± 2  
145 μm, fiber length 230 ± 23 μm, fiber density 1.8 g/cm<sup>3</sup> [45])

146 (3) Pitch CFR PEEK (density 1.4 g/cm<sup>3</sup>, PEEK-OPTIMA™ LT1 matrix with 30% wt  
147 Pitch carbon fibers, tradename PEEK-OPTIMA Wear Performance™, Invibio,  
148 Lankashire, UK). Fibers are short and randomly distributed (fiber modulus 280 GPa,  
149 fiber diameter 10 ± 2 μm, fiber length 230 ± 13 μm, fiber density 2.0 g/cm<sup>3</sup> [45])

150 Material granules were obtained from Invibio and processed into dog-bone and compact-  
151 tension (CT) specimens (Figure 1). Granules were first pre-heated to 70°C to remove residual  
152 moisture then injection molded into plates (250 x 25 x 2.5 mm). The injection nozzle  
153 temperature was held constant at 400°C and the mold at 250°C. Samples were cooled in air at  
154 room temperature. Water-jet machining was used to cut dog-bone and CT specimens from the  
155 plates, with the samples oriented for load application parallel to the mold-fill direction.

156 Three heat treatments were examined to investigate the effects of post-processing thermal  
157 treatment on FCP behavior. Samples were either non-annealed, annealed at 200°C, or annealed  
158 at 300°C. Annealing was conducted for five hours in a Nabertherm oven (Lilienthal, Germany),

159 with an initial heating rate of 5°C/min. After annealing, samples were cooled in air at room  
160 temperature. Annealing was performed by Lima Corporate (Udine, Italy).

## 161 **2.2 Monotonic testing**

162 Tensile testing to failure was performed on non-heat-treated samples in accordance with  
163 ASTM D638 on type V dog-bone specimens (n=4 samples tested per material for a total of 12  
164 tests). Monotonic mechanical testing for equivalent heat-treated materials has been reported  
165 elsewhere [25,46] and was therefore not repeated here. Displacement was applied at a rate of 0.5  
166 mm/min in ambient conditions (21°C / 28% RH) using a screw-driven Instron (model 5500R).  
167 Strain was measured using a video extensometer (Instron, model 2663-821). Temperature of the  
168 gauge-section was not measured during monotonic testing. Due the viscoelastic nature of  
169 thermoplastic polymers, reported mechanical properties should be understood within the context  
170 of displacement rate and ambient temperature. However, it has been previously shown that at  
171 room temperature ( $\approx 124$  °C below PEEK's glass transition temperature), varying displacement  
172 rate by over four orders of magnitude (from 0.05 to 50 mm/min) had little effect on elastic  
173 modulus and increased yield stress by less than 1.4x [47].

174 Elastic modulus (E), ultimate tensile strength ( $\sigma_{ut}$ ), and elongation at failure ( $\epsilon_f$ ) were  
175 reported for each material. Elastic modulus was calculated using a secant approximation  
176 between 0.1% and 0.5% strain for each specimen. Student's t-tests were used to compare E,  $\sigma_{ut}$ ,  
177 and  $\epsilon_f$  between material formulations with significance assumed at  $p \leq 0.05$ .

## 178 **2.3 Fatigue testing**

179 Fatigue crack propagation (FCP) experiments were conducted on CT specimens using a  
180 servo-hydraulic Instron (model 8871) and a load-controlled sinusoidal wave function at a  
181 frequency of 5 Hz [41,43]. Testing was performed at room-temperature and an air-cooling

182 system was used to minimize hysteretic heating [48]. The load ratio (minimum load/maximum  
 183 load) was held constant at 0.1. A pre-crack of 1 mm was introduced at the tip of each notch  
 184 using a razor blade and custom fixture, and datum dots were placed on specimen sides for  
 185 subsequent image analysis [48]. Crack length was measured using a variable magnification  
 186 optical system (Infinivar CFM-2/S, 5 $\mu$ m/pixel) and a digital video camera (Sony XCD-SX910).  
 187 A custom LabView program controlled the camera, which captured images every 500 or 1000  
 188 cycles, depending on crack velocity. Custom scripts were created in ImageJ and MATLAB to  
 189 semi-automate data analysis. A minimum of three samples were tested for each material  
 190 formulation. The Paris equation (Equation 1) was used to map FCP as a function of cyclic stress  
 191 intensity, where  $da/dN$  is the rate of crack velocity (mm/cycle),  $\Delta K$  is the cyclic stress intensity  
 192 (i.e. the crack driving force, MPa $\sqrt{m}$ ), and C (pre-exponent) and m (exponent, slope on  
 193 logarithmic scale) are material constants. Any data not meeting the condition of small scale  
 194 yielding (Equation 2) were excluded from this analysis, where (W-a) is the uncracked ligament  
 195 length,  $K_{max}$  is the maximum mode-one stress intensity (MPa $\sqrt{m}$ ), and  $\sigma_{ys}$  is the material yield  
 196 strength (MPa).

$$197 \quad \left. \begin{array}{l} \frac{da}{dN} = C\Delta K^m \end{array} \right\} \text{Equation 1}$$

$$198 \quad (W - a) \geq \frac{4}{\pi} \left( \frac{K_{max}}{\sigma_{ys}} \right)^2 \quad \text{Equation 2}$$

## 199 **2.4 Fractography**

200 Fracture surfaces were imaged with scanning electron microscopy (SEM, Quanta FEI and  
 201 Versa 3D Dual Beam) at 50-500x and optical microscopy (Keyence VHX 6000) at 10-50x.  
 202 Some specimens were sputter coated in gold-vanadium to facilitate fracture surface visualization.

## 203 **3. Results**

### 204 **3.1 Monotonic testing results**

205 Compared with pitch CFR PEEK, PAN CFR PEEK exhibited a significantly higher  
206 elastic modulus ( $18.5 \pm 1.3$  vs  $12.5 \pm 1.3$  GPa, PAN vs pitch CFR PEEK,  $p = 0.006$ , AVG  $\pm$  SD)  
207 and ultimate tensile strength ( $192 \pm 17$  vs  $145 \pm 9$  MPa, PAN vs pitch CFR PEEK,  $p = 0.005$ ,  
208 AVG  $\pm$  SD) (Table 1). Strain at failure was not significantly different between fiber types ( $1.9 \pm$   
209  $0.2$  vs  $2.2 \pm 0.2$  % strain, PAN vs pitch CFR PEEK,  $p = 0.116$ , AVG  $\pm$  SD) (Table 1). Unfilled  
210 PEEK had a significantly lower elastic modulus ( $3.9 \pm 0.2$  GPa, AVG  $\pm$  SD) and ultimate tensile  
211 strength ( $93 \pm 1$  MPa), and a significantly higher strain at failure ( $66 \pm 7$  %, AVG  $\pm$  SD)  
212 compared with either fiber type ( $p \leq 0.002$ ) (Table 1). In terms of the stress-strain behavior,  
213 unfilled PEEK demonstrated appreciable post-yield deformation (necking), whereas both pitch  
214 and PAN CFR PEEK failed in a predominantly brittle manner, at low failure strains and with  
215 little post-yield deformation (Figure 2).

### 216 **3.2 Fatigue testing results**

217 The crack velocity ( $da/dN$ ) versus cyclic stress intensity ( $\Delta K$ ) curves for all PEEK  
218 materials generally followed a linear relationship in log-log space as described by the Paris Law  
219 (Equation 1, Figure 3). The region of stable crack growth was measured as  $3.2 \leq \Delta K \leq 7.1$   
220  $MPa\sqrt{m}$  for unfilled PEEK,  $4.2 \leq \Delta K \leq 6.8$   $MPa\sqrt{m}$  for pitch CFR PEEK, and  $4.6 \leq \Delta K \leq 8.6$   
221  $MPa\sqrt{m}$  for PAN CFR PEEK (all heat treatments). A rightward shift was observed in the PAN  
222 CFR PEEK data compared with the pitch CFR and unfilled PEEK data (all heat treatments).  
223 This rightward shift suggests an improvement in FCP resistance—a larger cyclic stress intensity  
224 was required to propagate a crack at a given velocity. The effect of annealing on FCP behavior  
225 appears small for unfilled and pitch CFR PEEK, evidenced by largely overlapping  $da/dN$  versus  
226  $\Delta K$  data (Figure 3). Annealing at  $300$  °C appears to have a more pronounced effect for PAN

227 CFR PEEK, evidenced by the distinct  $da/dN$  versus  $\Delta K$  data between PAN and PAN 300 (Figure  
228 3).

229 To clarify and quantify these observations, least squares regression analysis was used to  
230 generate best fit lines of the data (Figure 4).  $\Delta K$  values at a constant crack velocity of  $da/dN = 2$   
231  $\times 10^{-4}$  mm/cycle were compared in order to quantify the relative resistance to FCP as well as the  
232 effect of annealing at an intermediate crack velocity (Table 2). The value of  $da/dN = 2 \times 10^{-4}$   
233 mm/cycle was chosen because it represents a crack velocity approximately centered within the  
234 linear (Paris) growth regime, approximately halfway between near-threshold and near fast-  
235 fracture regions based on the spread of the measured data (Figure 3, Figure 4). For non-annealed  
236 formulations, propagating a crack at  $da/dN = 2 \times 10^{-4}$  mm/cycle required  $\Delta K = 4.9$  MPa $\sqrt{m}$  for  
237 unfilled PEEK,  $\Delta K = 4.7$  MPa $\sqrt{m}$  for pitch CFR PEEK, and  $\Delta K = 5.7$  MPa $\sqrt{m}$  for PAN CFR  
238 PEEK (Table 2). Thus, non-annealed unfilled and pitch CFR PEEK require a similar  $\Delta K$  for  
239 intermediate crack velocities while non-annealed PAN CFR PEEK requires an increased  $\Delta K$  on  
240 the order of 17-21% compared with unfilled and pitch CFR PEEK, respectively. For  
241 formulations annealed at 300 °C, the  $\Delta K$  values required to propagate a crack at  $da/dN = 2 \times 10^{-4}$   
242 mm/cycle remain similar between unfilled and pitch CFR PEEK (4.7 versus 4.8 MPa $\sqrt{m}$ ,  
243 respectively) but increased to 7.0 MPa $\sqrt{m}$  for PAN CFR PEEK, representing an increase of 45-  
244 50%.

245 The effect of heat-treatment on FCP resistance was thus relatively minor for unfilled  
246 PEEK, with a maximum  $\Delta K$  variation of 0.3 MPa $\sqrt{m}$  (6%) amongst heat treatments at  $da/dN = 2$   
247  $\times 10^{-4}$  mm/cycle. Similarly, the effect of heat treatment was relatively minor for pitch CFR  
248 PEEK, with a maximum  $\Delta K$  variation of 0.5 MPa $\sqrt{m}$  (9%) amongst heat treatments at  $da/dN = 2$   
249  $\times 10^{-4}$  mm/cycle. Conversely, heat-treatment had a larger effect on PAN CFR PEEK, with a

250 maximum  $\Delta K$  variation of 1.5 MPa $\sqrt{\text{m}}$  (24%) amongst heat treatments at  $da/dN = 2 \times 10^{-4}$   
251 mm/cycle.

252 The linear regression analysis also enabled calculation of the Paris exponent ( $m$  in  
253 Equation 1), a material-specific parameter describing the rate of crack acceleration. Larger  
254 values of  $m$  indicate larger rates of crack accelerations. Values of  $m$  ranged between 4 - 5.1 for  
255 unfilled PEEK, 6.6 – 8.0 for pitch CFR PEEK, and 5.9 – 6.3 for PAN CFR PEEK (Figure 5).  
256 Thus, we observe a trend towards larger values of crack acceleration for both pitch and PAN  
257 CFR PEEK compared with unfilled PEEK, suggesting that the addition of carbon-fibers can  
258 increase the rate of crack acceleration. Heat-treatment appeared to have a minor and non-  
259 constant effect on  $m$  (Figure 5). In unfilled and pitch CFR PEEK, annealing decreased  $m$ ,  
260 whereas for PAN CFR PEEK, annealing at 200 °C and 300 °C resulted in an increase in  $m$  of  
261 17% and 7%, respectively (6.9 and 6.3 versus 5.9).

### 262 **3.3 Fractography**

263 Under monotonic loading, the fracture surface of unfilled PEEK displayed macroscopic  
264 plastic deformation including tearing features and a reduced cross-sectional area at the location  
265 of fracture (a result of necking) (Figure 6). The fracture surfaces of pitch and PAN CFR PEEK  
266 were similar to each other, displaying little bulk plastic deformation in comparison with unfilled  
267 PEEK (Figure 6). Pitch and PAN CFR PEEK display fiber fracture and fiber pull-out throughout  
268 the fracture surface (Figure 6).

269 Under fatigue loading, unfilled PEEK exhibited striation-like markings and parabolic  
270 features in the stable growth regime (Figure 7). The parabolic features tended to grow larger at  
271 longer crack lengths (Figure 7E). Compared with the stable growth region, the unstable growth

272 region in unfilled PEEK exhibited much greater amounts of plastic deformation, evidenced by  
273 localized contraction (necking) around the crack tip (Figure 7A).

274 Pitch and PAN CFR PEEK present with little macroscopic deformation (Figure 8),  
275 resulting from suppression of plastic deformation due to the presence of carbon fibers. During  
276 stable FCP, some fiber fracture and pull-out were observed in combination with near-tip local  
277 deformation of the matrix material (Figure 8B, 8E). During unstable FCP, these local matrix  
278 deformation features are not observed and the fracture surfaces instead display primarily fiber  
279 fracture and fiber pull-out (Figure 8C, 8F).

280 There were no observable fractographic distinctions in macroscopic (reinforcement-level)  
281 failure mode or mechanism between heat-treatments for unfilled PEEK and pitch and PAN CFR  
282 PEEK. Higher imaging magnifications may illuminate crystalline-level mechanisms and  
283 warrants further investigation.

#### 284 **4. Discussion**

285 It was the aim of the current study was to investigate the effects of PAN- and pitch-based  
286 carbon fibers on the monotonic properties and FCP resistance of orthopedic grade PEEK.  
287 Additionally, we sought to elucidate the effects of annealing on FCP resistance.

288 Complete crystallinity data for the materials used in this study have been reported  
289 elsewhere [25]. Briefly, crystallinity for non-annealed PEEK is  $\approx 32\%$ , and all non-annealed  
290 formulations (i.e. unfilled, pitch and PAN CFR PEEK) are within 1% of this value [25].  
291 Annealing enhances crystallinity in unfilled and pitch and PAN CFR PEEK by similar amounts:  
292 Low temperature (200 °C) annealing enhances crystallinity by  $\approx 1\%$  while high temperature (300  
293 °C) annealing enhances crystallinity by  $\approx 9\%$  [25].

294 The addition of both pitch and PAN carbon fibers to the PEEK matrix increased  
295 monotonic stiffness and strength and decreased ductility (strain to failure) compared with  
296 unfilled PEEK. These trends are consistent with data published by the material manufacturer  
297 [26,49,50] and with the behavior of many short-fiber thermoplastic polymer composites.  
298 Comparing fiber types, we observed statistically significant increases of 48% in elastic modulus  
299 and 32% in ultimate tensile strength, and a non-statistically significant decrease of 14% in strain  
300 to failure for PAN versus pitch CFR PEEK. Increases in elastic modulus and ultimate tensile are  
301 attributed to a number of microstructural characteristics, including inherent fiber mechanical  
302 properties, differences in fiber number, and differences in fiber aspect ratio. The PAN-based  
303 carbon fibers used in this study are 93% stiffer than pitch-based carbon fibers (elastic modulus  
304 540 versus 280 GPa, PAN- versus pitch-based carbon fibers, respectively) [29]. Thus, composite  
305 mechanical property differences would be expected even if other parameters (fiber number, fiber  
306 aspect ratio, interfacial bonding, crystallinity, etc.) were equivalent. Further, PAN-based carbon  
307 fibers are thinner and less dense than pitch-based carbon fibers (diameter 6 versus 10  $\mu\text{m}$ ,  
308 density 1.8 versus 2.0  $\text{g}/\text{cm}^3$ , PAN- versus pitch-based carbon fibers, respectively), and we thus  
309 expect  $\approx 3.1$  times more PAN-based carbon fibers in a given specimen compared with pitch-  
310 based carbon fibers for an equivalent wt % reinforcement (both composites used in this study  
311 contained 30% wt fiber reinforcement). In a related vein, since the diameter of PAN-based  
312 carbon fibers are smaller than pitch-based carbon fibers, the ratio of fiber surface area to fiber  
313 volume will be enhanced in PAN versus pitch CFR PEEK for an equivalent fiber volume  
314 fraction, thereby providing more surface area for the PEEK matrix to bond to PAN-based carbon  
315 fibers. We suggest that improvements in mechanical behavior for PAN versus pitch CFR PEEK  
316 are attributed to these compound effects: PAN-based carbon fibers are themselves stiffer, more

317 PAN-based carbon fibers are present, and comparatively more PAN-based carbon fiber surface  
318 area is exposed to PEEK matrix, thus enhancing the area available for fiber/matrix bonding.

319 Under fatigue loading, we found that the addition of pitch-based carbon fibers did not  
320 enhance FCP resistance, as the  $da/dN$  versus  $\Delta K$  behavior for unfilled and pitch CFR PEEK are  
321 similar. FCP resistance of these materials was largely unaffected by either low-temperature (200  
322 °C) or high-temperature (300 °C) annealing. Conversely, the FCP resistance of PAN CFR PEEK  
323 was appreciably improved compared with unfilled and pitch CFR PEEK. For non and low-  
324 temperature annealed PAN CFR PEEK, the improvement was on the order of 17-21%, while for  
325 high-temperature annealed PAN CFR PEEK the improvement was on the order of 45-50% at an  
326 intermediate crack velocity.

327 The complex interdependence of microstructural parameters including manufacturing-  
328 and annealing-induced matrix crystallinity, fiber type, fiber number, and fiber aspect ratio,  
329 coupled with complex dynamics of FCP in polymer composites, make it difficult to  
330 unambiguously differentiate individual microstructural effects on FCP behavior. Yet, a number  
331 of observations warrant discussion.

332 The addition of fibers to a polymer matrix can enhance resistance to FCP by introducing  
333 energy dissipation mechanisms via fiber fracture and pull-out [44]. Simultaneously, fibers can  
334 inhibit energy dissipation by limiting the ability of the matrix to deform plastically [44]. The  
335 balance between net energy dissipation/absorption (thus FCP improvement/degradation) depends  
336 on a balance between matrix ductility (which depends on matrix molecular weight, crystallinity,  
337 etc.), fiber properties, and the properties of the fiber/matrix interface. Previous studies have  
338 shown that the addition of 30% wt. randomly distributed short glass fibers to a PEEK matrix  
339 provided little to no improvement in FCP resistance, while the addition of 30% wt. randomly

340 distributed carbon fibers provided at least some improvement in FCP resistance [36,41,43] (the  
341 carbon fiber type is not mentioned in these studies, however PAN-based carbon fibers are the  
342 likely historical precedent [51]). This phenomenon is attributed to stronger fiber/matrix adhesion  
343 between the carbon fibers and the PEEK matrix compared with glass fibers and the PEEK matrix  
344 [36,41,44]. The results found in the current study, in which the addition of pitch-based carbon  
345 fibers provided little to no improvement in FCP resistance, while the addition of PAN-based  
346 carbon fibers provided an appreciable improvement in FCP resistance, could be plausibly  
347 explained via the same mechanism; stronger fiber/matrix adhesion in PAN- compared with pitch-  
348 based PEEK composites. However, aforementioned differences in inherent fiber properties, fiber  
349 numbers, and fiber aspect ratios confound and preclude a definitive statement on interfacial bond  
350 strength. Indeed, the fact that observed improvements in FCP resistance for PAN CFR PEEK  
351 are not commensurate with the magnitude of differences in fiber properties or fiber number could  
352 plausibly suggest a weaker interfacial bond for PAN versus pitch CFR PEEK. Additional studies  
353 are required to clarify differences in interfacial bond strength, which could be achieved via FCP  
354 tests controlling for fiber aspect ratio and/or fiber number.

355         Annealing has been shown to have a greater impact on FCP resistance for CFR PEEK  
356 compared with unfilled PEEK (carbon fiber type not specified), even when similar overall  
357 increases in crystallinity are induced by annealing [36,41]. Results found in the current study for  
358 PAN CFR PEEK are similar—annealing had no measurable effect on unfilled PEEK but  
359 appreciably improved FCP resistance in PAN CFR PEEK. It has been suggested that annealing  
360 may preferentially influence the matrix in regions near the fiber/matrix interface [36]. Thus,  
361 while it is not clear why annealing had no measurable effect on pitch CFR PEEK, one plausible  
362 explanation is that a lower fiber number in pitch versus PAN CFR PEEK (thus fewer

363 fiber/matrix interfacial regions) makes any preferential improvements in crystallinity less  
364 pronounced. It has also been suggested that annealing enhances crystalline growth of the PEEK  
365 matrix onto the carbon fiber surface, thereby improving interfacial bond strength [41]. Thus, a  
366 second and related explanation follows that differences in crystallization mechanisms between  
367 PAN and pitch CFR PEEK [45] contribute to differences in interfacial bond strength as a  
368 function of annealing, even for similar overall degrees of crystallinity.

369 Fractographic analysis of failure surfaces suggest two distinct modes of FCP in PEEK,  
370 notably a cyclic mode acting at low crack growth rates and a static mode acting at high crack  
371 growth rates, as described by previous studies [37,38,40,43,44].

372 In unfilled PEEK, the stable growth regime exhibited striation-like markings (Figure 7B,  
373 7C), similar to those reported previously [37,38,40,41,44], presumably caused by crack blunting  
374 and re-sharpening during cyclic loading. The average width of the striation-like bands were not  
375 measured in this study and compared to  $da/dN$  to confirm whether they were true fatigue  
376 striations. Yet, previous investigations [37,40,41] confirmed markings of similar size and  
377 morphology to be true fatigue striations. The observed parabolic features (Figure 7C, 7E) are  
378 also consistent with previous investigations [37,41,44], and are attributed to the intersection of  
379 the primary crack front with secondary cracks induced by inherent flaws. Unlike the stable  
380 growth regime, the fast-fracture regime in unfilled PEEK is characterized by ductile contraction  
381 (i.e. necking) in the zone around the crack tip. This ductile contraction in fast fracture region is  
382 not apparent during stable crack growth but is apparent for monotonically tested PEEK.

383 Failure surfaces of pitch and PAN CFR PEEK also show evidence of an interaction  
384 between cyclic and static mechanisms during FCP in line with previous studies on CFR PEEK  
385 [44]. At low crack growth rates, we observe regions of matrix deformation and rupture near to

386 and along the fiber/matrix interface, as well as fiber fracture and pull-out (Figure 8B, 8E). It has  
387 been previously shown that under cyclic loading, local failure is dominated by separation along  
388 the fiber/matrix interfaces and rupture of the matrix material between fibers [36,43]. At higher  
389 crack growth rates, equivalent matrix deformation is not observed, and the fracture surface is  
390 instead comprised primarily of fiber fracture and pull-out (Figure 8C, 8F) more akin to  
391 monotonically tested samples (Figure 6). Thus, our findings offer supporting evidence for cyclic  
392 modes of growth at low growth rates which transition to static modes near the onset of failure in  
393 unfilled and both pitch and PAN CFR PEEK.

394 While the CFR PEEK formulations used in this study were reinforced using short,  
395 randomly distributed fibers to achieve bulk isotropy, the injection molding process has been  
396 shown to introduce some fiber alignment in proximity to the specimen surface (i.e. a “skin”  
397 layer) induced by friction with the mold wall [29,36,41,43,44]. This well-documented skin-core  
398 structure has been shown to produce more rapid crack growth when load is applied perpendicular  
399 to the mold-fill direction (thus crack growth parallel to the mold-fill direction) compared with the  
400 converse orientation [43,44]. Thus, the results here are limited to load application parallel to the  
401 mold fill direction.

## 402 **5. Conclusion**

403 Under monotonic loading, PAN CFR PEEK exhibited a larger elastic modulus and  
404 ultimate tensile strength compared with unfilled and pitch CFR PEEK. Under cyclic loading,  
405 PAN CFR PEEK exhibited an improved resistance to fatigue crack propagation compared with  
406 unfilled and pitch CFR PEEK. The improvement in fatigue crack propagation resistance for  
407 PAN CFR PEEK was enhanced following high-temperature (300 °C) annealing.

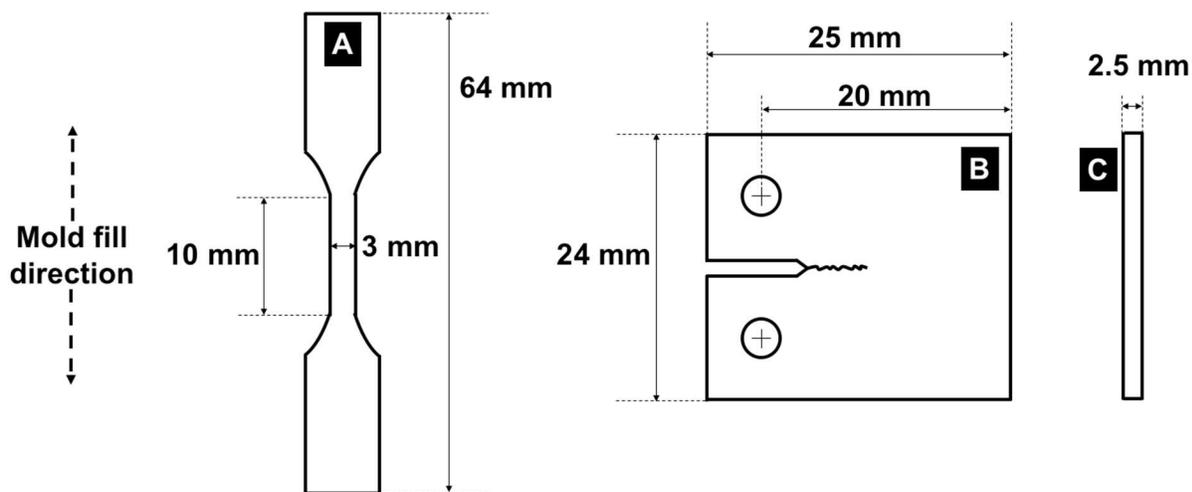
408 Pitch CFR PEEK did not exhibit improved fatigue crack propagation resistance compared  
409 with unfilled PEEK. Neither low temperature (200 °C) nor high temperature (300 °C) annealing  
410 produced a measurable effect on the fatigue crack propagation behavior of these materials.

411 The improvement in mechanical properties for PAN CFR PEEK is attributed to a  
412 compound effect: PAN-based carbon fibers are themselves stiffer than pitch-based carbon fibers,  
413 more PAN-based carbon fibers are present compared with pitch-based carbon fibers for an  
414 equivalent wt % reinforcement, and comparatively more PAN-based carbon fiber surface area is  
415 exposed to PEEK matrix, thus enhancing the area available for fiber/matrix bonding.  
416 Differences in fiber/matrix interfacial bond strength between PAN- versus pitch-based carbon  
417 fibers should be further elucidated, possibly via studies controlling for fiber number and/or  
418 aspect ratio.

419 Fatigue crack propagation was shown to proceed via cyclic modes during stable crack  
420 growth, characterized by striation-like bands and parabolic features in unfilled PEEK and matrix  
421 rupture near to and along the fiber/matrix interface in pitch and PAN CFR PEEK. Cyclic modes  
422 transition to static modes (more akin to monotonic fracture) at longer crack lengths,  
423 characterized by necking in unfilled PEEK and an increased degree of fiber fracture and pull-out  
424 in pitch and PAN CFR PEEK. The mechanisms of fatigue crack propagation appear similar  
425 between carbon-fiber types.

426

## 427 6. Figures and Tables



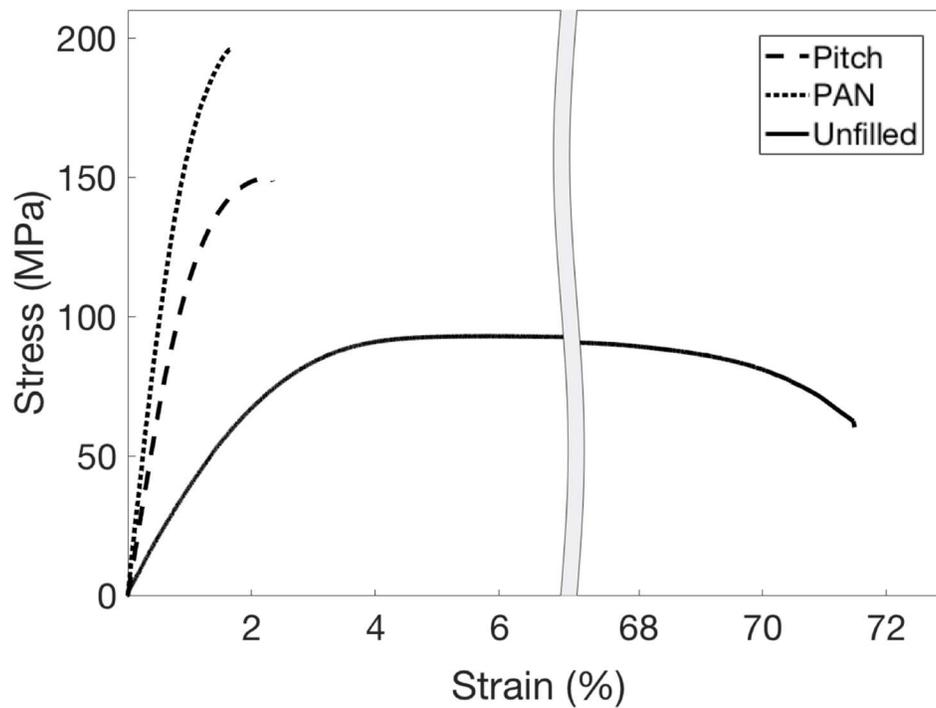
428  
 429 Figure 1. A) ASTM D638 type V dog-bone specimens used for monotonic testing. B) Compact-  
 430 tension (CT) specimen used for FCP testing. C) Thickness for all specimens. Samples were  
 431 oriented for load application parallel to the mold fill direction. Drawings are not to scale.

432  
 433  
 434  
 435  
 436

Table 1. Material properties for PEEK materials (non-heat-treated formulations).

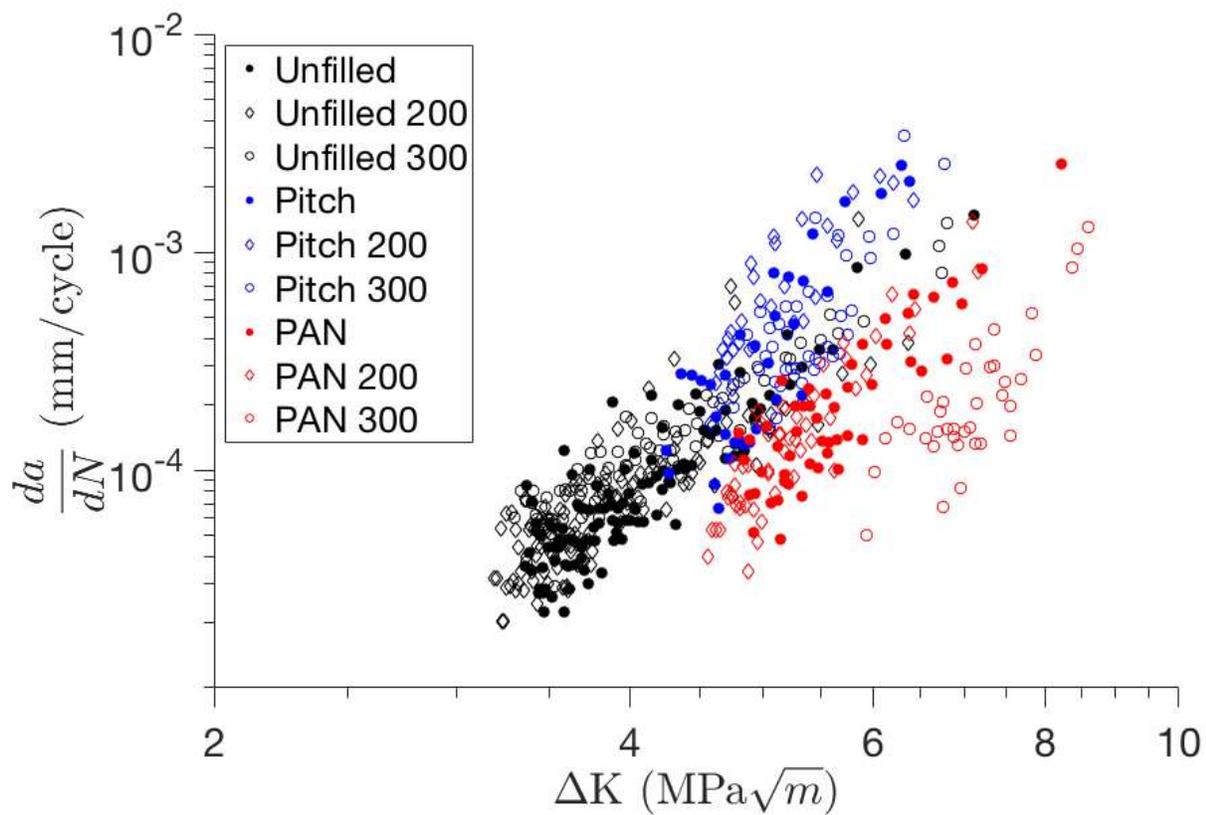
	Unfilled	Pitch	PAN
E (GPa)	$3.9 \pm 0.2$	$12.5 \pm 1.3$	$18.5 \pm 2.3$
$\sigma_{ut}$ (MPa)	$93 \pm 1$	$145 \pm 9$	$192 \pm 17$
$\epsilon_f$ (%)	$66 \pm 7$	$2.2 \pm 0.2$	$1.9 \pm 0.2$

437



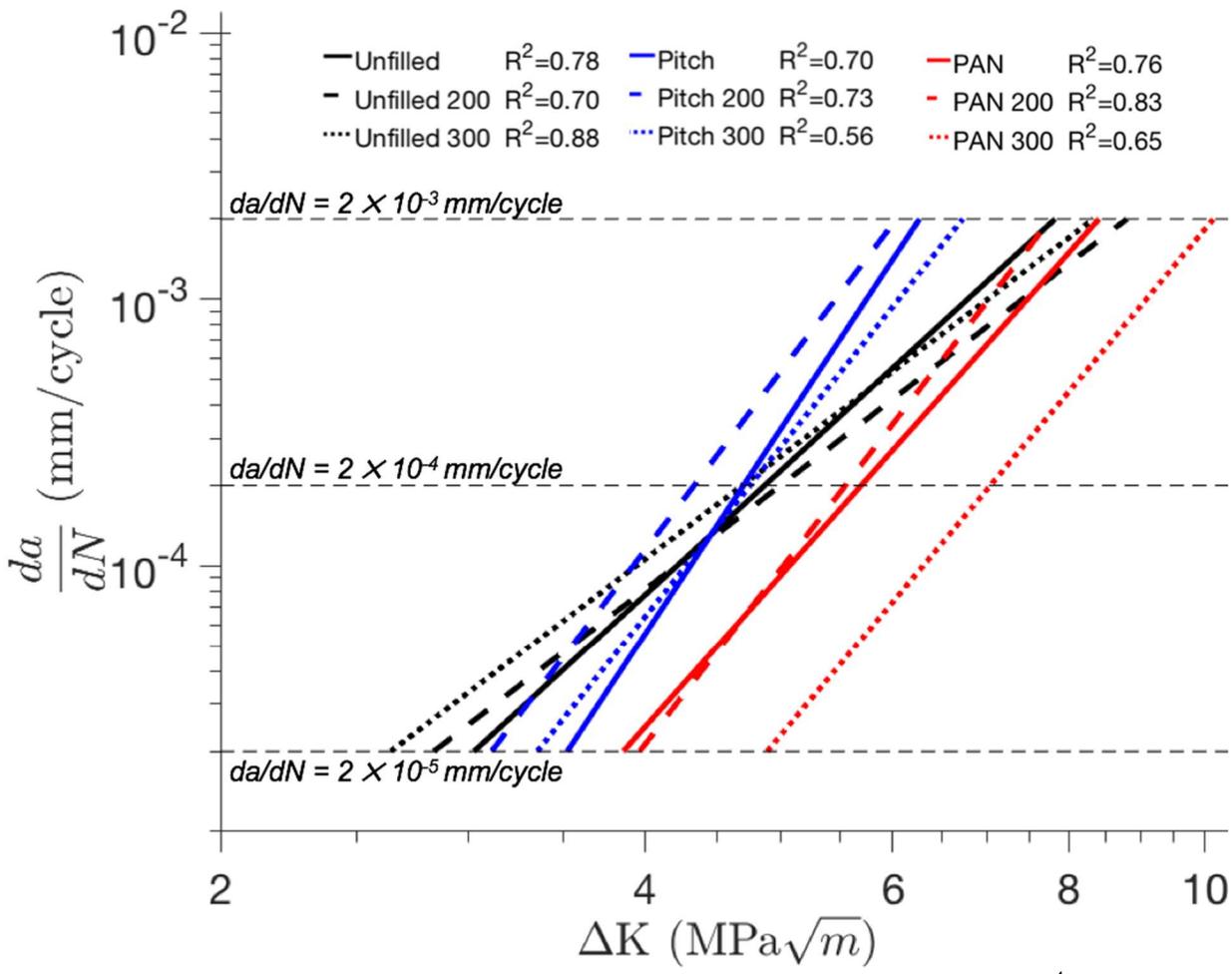
438  
439  
440  
441  
442  
443

Figure 2. Representative stress-strain plots for Pitch CFR PEEK, PAN CFR PEEK, and unfilled PEEK (non heat-treated formulations).



444

445 Figure 3. FCP plots for all material formulations and heat-treatments.



446  
447  
448  
449  
450  
451  
452  
453  
454  
455  
456  
457  
458  
459  
460  
461  
462  
463  
464  
465  
466

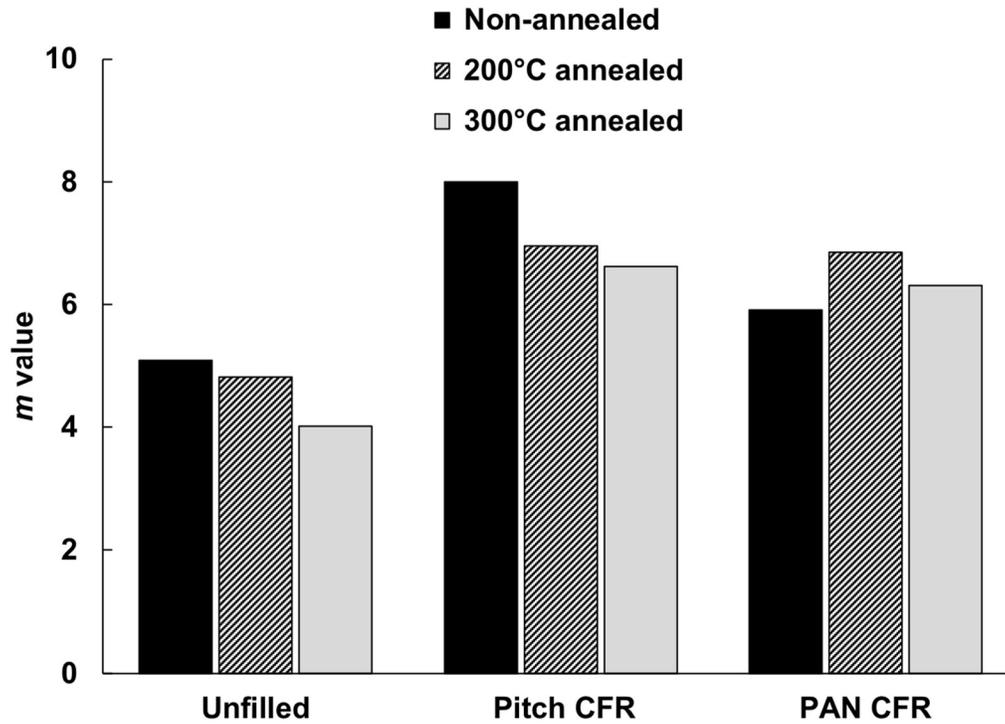
Figure 4. Paris fits for all materials. A constant crack velocity of  $da/dN = 2 \times 10^{-4}$  mm/cycle was chosen to represent an intermediate crack velocity.

467  
468  
469

Table 2.  $\Delta K$  values at the intermediate crack velocity of  $da/dN = 2 \times 10^{-4}$  mm/cycle for all materials.

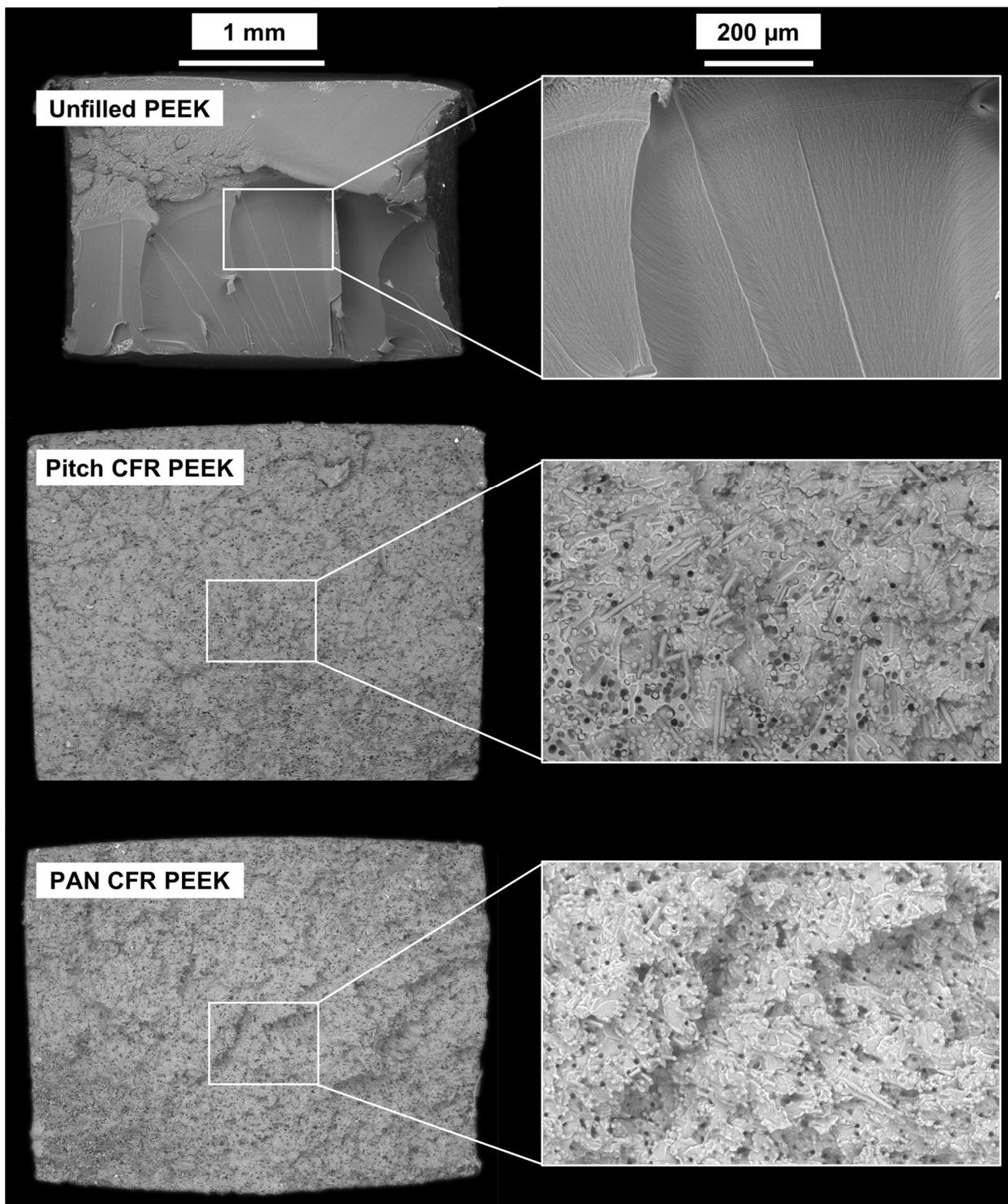
<b><math>\Delta K</math> (MPa<math>\sqrt{m}</math>) at <math>da/dN = 2 \times 10^{-4}</math> mm/cycle</b>	
<b>Unfilled</b>	
0 °C	4.9
200 °C	5.0
300 °C	4.7
<b>Pitch</b>	
0 °C	4.7
200 °C	4.3
300 °C	4.8
<b>PAN</b>	
0 °C	5.7
200 °C	5.6
300 °C	7.0

470  
471  
472  
473

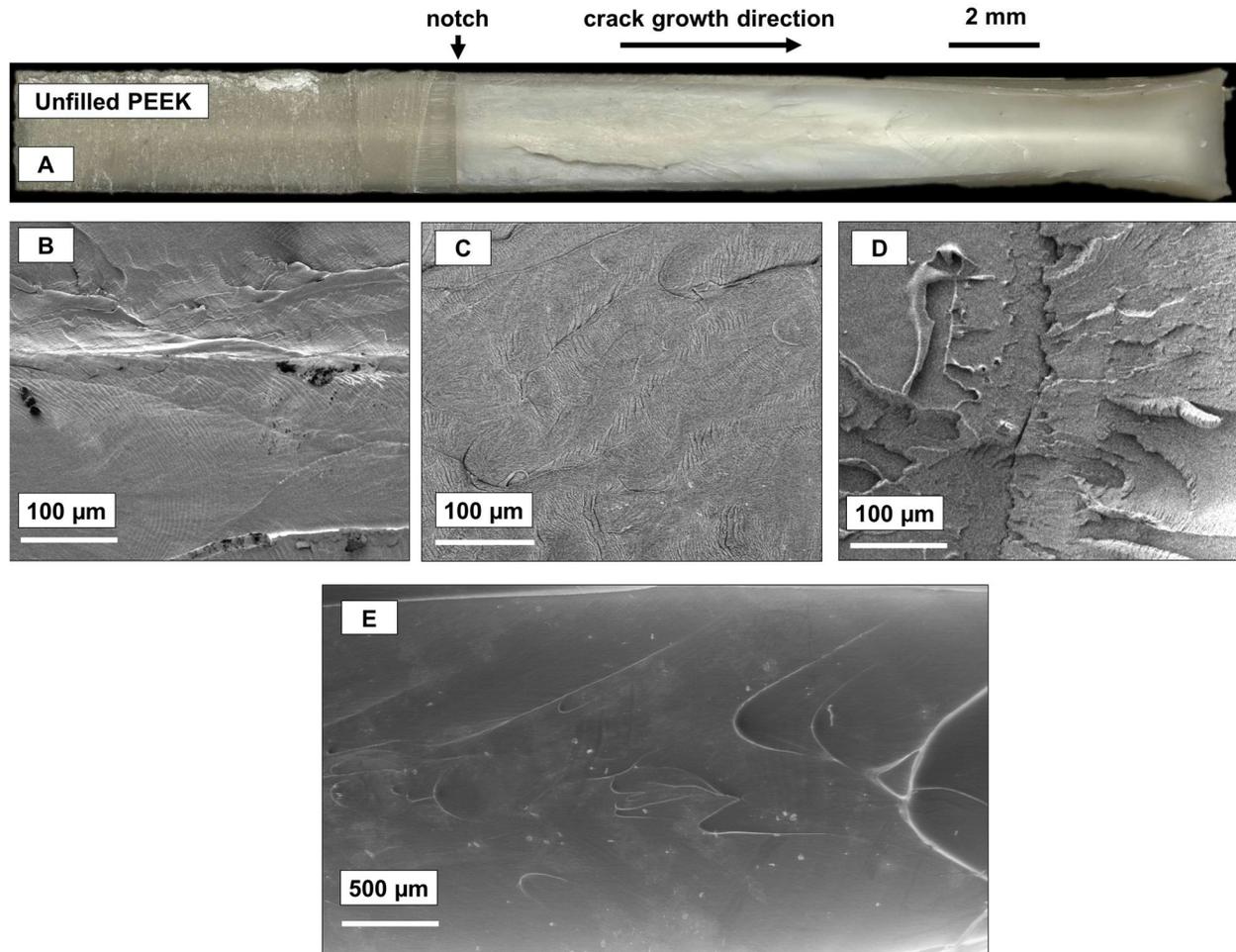


474  
475  
476

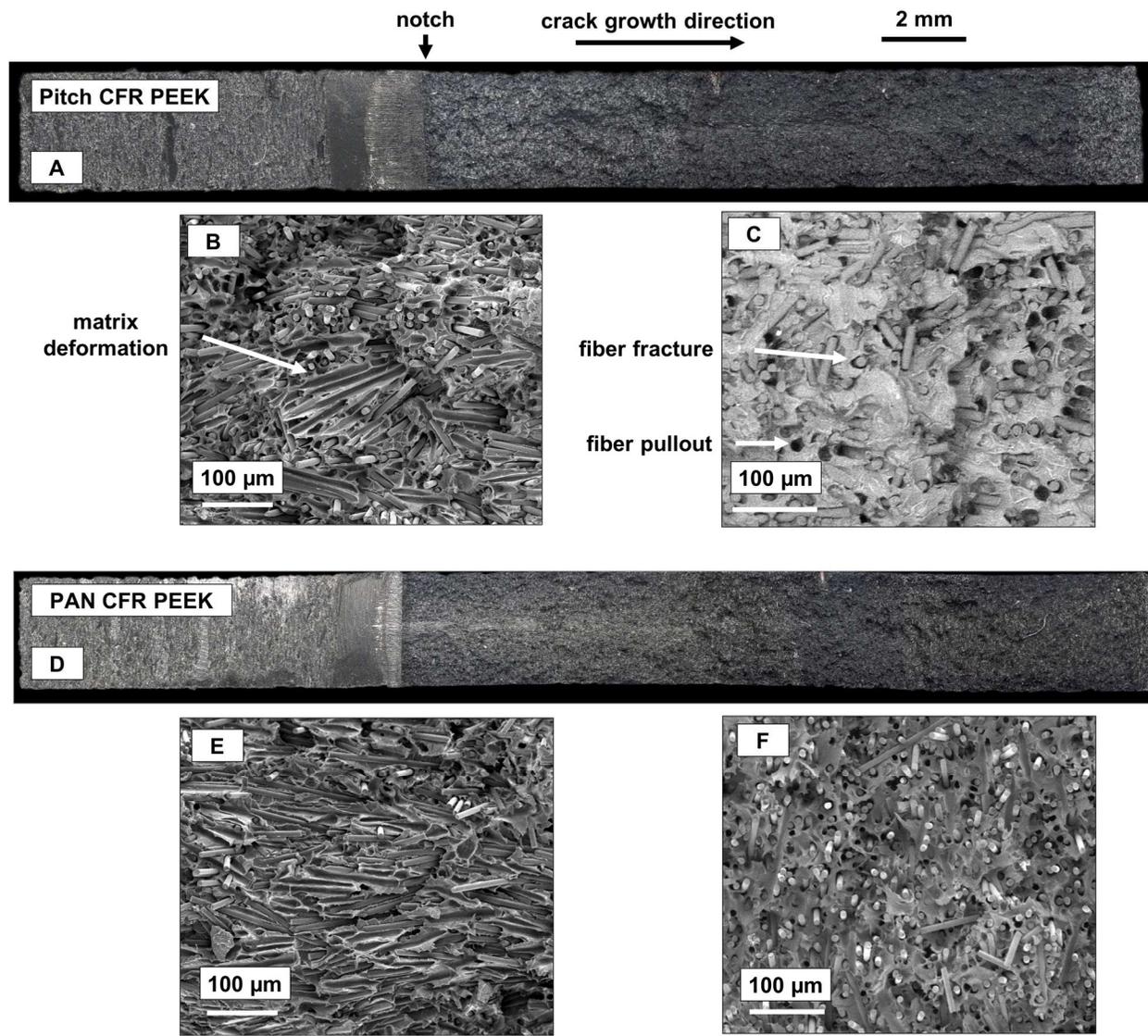
Figure 5. Paris constant,  $m$ , describing the rate of crack acceleration (slope of the  $da/dN$  versus  $\Delta K$  plot) for all material formulations and heat-treatments.



477  
478 Figure 6. SEM images of the fracture surfaces of monotonically tested samples (non-heat-treated  
479 formulations).



480  
 481 Figure 7. Images of the fracture surfaces of fatigue tested unfilled PEEK (non-heat-treated  
 482 formulations). B: Early growth region. C: Mid growth region. D: Fast fracture region. E: Mid-  
 483 to-late growth region.



484  
 485 Figure 8. Images of the fracture surfaces of fatigue tested pitch (top) and PAN (bottom) CFR  
 486 PEEK (non-heat-treated formulations). B and E: Early growth region. C and F: Fast fracture  
 487 region.  
 488

## 489 7. Acknowledgements

490 The authors would like to acknowledge Limacorporate SpA for material and manufacturing  
491 support.

## 492 8. Bibliography

- 493 [1] Kurtz S. An Overview of PEEK Biomaterials. In: Kurtz S, editor. PEEK Biomaterials  
494 Handbook. 2012. p. 1–7.
- 495 [2] Kurtz S, Devine J. PEEK biomaterials in trauma, orthopedic, and spinal implants.  
496 *Biomaterials*. 2007;28(32):4845–69.
- 497 [3] Kumar S, Anderson D, Adams W. Crystallization and Morphology of Poly(aryl-ether-  
498 ether-ketone). *Polymer (Guildf)*. 1986;27:329–36.
- 499 [4] Reitman M, Jaekel D, Siskey R, et al. Morphology and crystalline architecture of  
500 polyaryletherketones. In: Kurtz S, editor. PEEK Biomaterials Handbook. 2012. p. 49–60.
- 501 [5] Green S, Schlegel J. A Polyaryletherketone Biomaterial for use in Medical Implant  
502 Applications. In: Polymers for the Medical Industry, Proceedings of a Conference held in  
503 Brussels. 2001. p. 1–7.
- 504 [6] Blundell D, Osborn B. The Morphology of Poly(aryl-ether-ether-ketone). *Polymer*  
505 *(Guildf)*. 1983;24:953–8.
- 506 [7] Tung C, Dynes P. Morphological characterization of polyetheretherketone-carbon fiber  
507 composites. *J Appl Polym Sci*. 1987;33:505–20.
- 508 [8] Mehmet-Alkan A, Hay J. The Crystallinity of PEEK Composites. *Polymer (Guildf)*.  
509 1993;34(16):3529–31.
- 510 [9] Velisaris C, Seferis J. Heat Transfer Effects on the Processing-Structure Relationships of  
511 Polyetheretherketone (PEEK) Based Composites. *Polym Eng Sci*. 1988;28(9):583–91.
- 512 [10] Ernstberger T, Buchhorn G, Heidrich G. Artifacts in spine magnetic resonance imaging  
513 due to different intervertebral test spacers. *Neuroradiology*. 2008;51:525–9.
- 514 [11] Panfil E, Pierdicca L, Salvolini L, et al. Magnetic resonance imaging (MRI) artefacts in  
515 hip prostheses: A comparison of different prosthetic compositions. *Radiol Medica*.  
516 2014;119:113–20.
- 517 [12] Brantigan J, Steffee A. A Carbon Fiber Implant to Aid Interbody Lumbar Fusion: Two-  
518 Year Clinical Results in the First 26 Patients. *Spine (Phila Pa 1976)*. 1993;18(14):2106–  
519 17.
- 520 [13] Sastri V. High-Temperature Engineering Thermoplastics: Polysulfones, Polyimides,  
521 Polysulfides, Polyketones, Liquid Crystalline Polymers, and Fluoropolymers. In: *Plastics*  
522 *in Medical Devices*. 2nd ed. 2014. p. 173–213.
- 523 [14] Kurtz S. Applications of polyaryletheretherketone in spinal implants. In: Kurtz S, editor.  
524 PEEK Biomaterials Handbook. 2012. p. 231–51.
- 525 [15] Rotini R, Cavaciocchi M, Fabbri D, et al. Proximal Humeral Fracture Fixation:  
526 Multicenter Study with Carbon Fiber PEEK Plate. *Musculoskelet Surg*. 2015;99:1–8.
- 527 [16] Schliemann B, Hartensuer R, Koch T, et al. Treatment of Proximal Humerus Fractures  
528 with a CFR-PEEK Plate: 2-year Results of a Prospective Study and Comparison to  
529 Fixation with a Conventional Locking Plate. *J Shoulder Elb Surg*. 2015;1282–8.
- 530 [17] Akhavan S, Matthiesen M, Schulte L, et al. Clinical and histologic results related to a low-  
531 modulus composite total hip replacement stem. *J Bone Jt Surg*. 2006;88:1308–14.

- 532 [18] Glassman A. Composite femoral stem for total hip arthroplasty. *Curr Opin Orthop.*  
533 2008;19(1):6–10.
- 534 [19] Uthoff H, Poitras P, Backman D. Internal Plate Fixation of Fractures: Short History and  
535 Recent Developments. *J Orthop Sci.* 2006;11:118–26.
- 536 [20] Bugbee W, Culpepper W, Engh C, et al. Long-Term Clinical Consequences of Stress-  
537 Shielding After Total Hip Arthroplasty Without Cement. *J Bone Jt Surg.*  
538 1997;79(7):1007–12.
- 539 [21] Reilly D, Burstein A. The elastic and ultimate properties of compact bone tissue. *J*  
540 *Biomech.* 1975;8(6).
- 541 [22] Li C, Vannabouathong C, Sprague S, et al. The use of carbon-fiber-reinforced (CFR)  
542 PEEK material in orthopedic implants: A systematic review. *Clin Med Insights Arthritis*  
543 *Musculoskelet Disord.* 2014;8:33–45.
- 544 [23] Wang A, Lin R, Stark C, et al. Suitability and limitations of carbon fiber reinforced PEEK  
545 composites as bearing surfaces for total joint replacements. *Wear.* 1999;225–229:724–7.
- 546 [24] Polineni V, Wang A, Essner A, et al. Characterization of Carbon Fiber-Reinforced PEEK  
547 Composite for use as a Bearing Material in Total Hip Replacements. *ASTM Int.* 1998;266–  
548 73.
- 549 [25] Regis M, Lanzutti A, Bracco P, et al. Wear behavior of medical grade PEEK and CFR  
550 PEEK under dry and bovine serum conditions. *Wear.* 2018;408–409(May):86–95.
- 551 [26] Invibio. PEEK-OPTIMA Wear Performance: Typical Material Properties [Internet]. 2013  
552 [cited 2016 May 2]. Available from: [https://invibio.com/ortho/materials/peek-optima-](https://invibio.com/ortho/materials/peek-optima-wear-performance)  
553 [wear-performance](https://invibio.com/ortho/materials/peek-optima-wear-performance)
- 554 [27] Flock J, Friedrich K, Yuan Q. On the friction and wear behaviour of PAN-and pitch-  
555 carbon fiber reinforced PEEK composites. *Wear.* 1999;225–229:304–11.
- 556 [28] Huang X. Fabrication and properties of carbon fibers. *Materials (Basel).* 2009;2(4):2369–  
557 403.
- 558 [29] Regis M, Fusi S, Favaloro R, et al. CFR PEEK composites for orthopaedic applications.  
559 In: 9th International Conference on Composite Science and Technology. 2013.
- 560 [30] Yuan Q, Bateman S, Friedrich K. Thermal and mechanical properties of PAN- and pitch-  
561 based carbon fiber reinforced PEEK composites. *J Thermoplast Compos Mater.*  
562 2008;21(4):323–36.
- 563 [31] Sardar Z, Jarzem P. Failure of a Carbon Fiber-Reinforced Polymer Implant Used for  
564 Transforaminal Lumbar Interbody Fusion. *Glob Spine J.* 2013;3(4):253–6.
- 565 [32] Tullberg T. Failure of a Carbon Fiber Implant. A Case Report. *Spine (Phila Pa 1976).*  
566 1998;23(16):1804–6.
- 567 [33] Ansari F, Chang J, Huddleston J, et al. Fractography and oxidative analysis of gamma  
568 inert sterilized posterior-stabilized tibial insert post fractures: Report of two cases. *Knee.*  
569 2013;20(6):609–13.
- 570 [34] Tower A, Currier J, Currier B, et al. Rim Cracking of the Cross-Linked After Total Hip  
571 Arthroplasty. *J Bone Jt Surg.* 2007;2212–7.
- 572 [35] Bonnheim N, Gramling H, Ries M, et al. Fatigue fracture of a cemented Omnifit CoCr  
573 femoral stem: implant and failure analysis. *Arthroplast Today.* 2017;3:234–8.
- 574 [36] Saib K, Isaac D, Evans W. Effects of processing variables on fatigue in molded PEEK and  
575 its short fiber composites. *Mater Manuf Process.* 1994;9(5):829–50.
- 576 [37] Saib K, Evans W, Isaac D. The role of microstructure during fatigue crack growth in poly  
577 (aryl ether ether ketone) (PEEK). *Polymer (Guildf).* 1993;34(15):3198–203.

- 578 [38] Brillhart M, Botsis J. Fatigue crack growth analysis in PEEK. *Int J Fatigue*. 1994;16:134–  
579 40.
- 580 [39] Brillhart M, Botsis J. Fatigue fracture behavior of PEEK: 2. Effects of thickness and  
581 temperature. *Polymer (Guildf)*. 1992;33(24):5225–32.
- 582 [40] Brillhart M, Gregory B, Botsis J. Fatigue fracture behavior of PEEK: 1. Effects of load  
583 level. *Polymer (Guildf)*. 1991;32(9):1605–11.
- 584 [41] Karger-Kocsis J, Walter R, Friedrich K. Annealing effects on the fatigue crack  
585 propagation of injection-moulded PEEK and its short fibre composites. *J Polym Eng*.  
586 1988;8(3–4):221–53.
- 587 [42] Chu J, Schultz J. The influence of microstructure on the failure behaviour of PEEK. *J*  
588 *Mater Sci*. 1990;25:3746–52.
- 589 [43] Friedrich K, Walter R, Voss H, et al. Effect of short fibre reinforcement on the fatigue  
590 crack propagation and fracture of PEEK-matrix composites. *Composites*. 1986;17(3):205–  
591 16.
- 592 [44] Evans W, Isaac D, Saib K. The effect of short carbon fibre reinforcement on fatigue crack  
593 growth in PEEK. *Composites*. 1996;27A:547–54.
- 594 [45] Regis M, Zanetti M, Pressacco M, et al. Opposite role of different carbon fiber  
595 reinforcements on the non-isothermal crystallization behavior of poly(etheretherketone).  
596 *Mater Chem Phys*. Elsevier B.V; 2016;179:223–31.
- 597 [46] Regis M, Bellare A, Pascolini T, et al. Characterization of thermally annealed PEEK and  
598 CFR-PEEK composites. *Polym Degrad Stab*. 2017;136:121–30.
- 599 [47] Maksimov R, Kubat J. Time and temperature dependent deformation of poly(ether ether  
600 ketone) (PEEK). *Mech Compos Mater*. 1997;33(6):517–25.
- 601 [48] Ansari F. The Interplay of Design and Materials in Orthopedics: Evaluating the Impact of  
602 Notch Geometry on Fatigue Failure of UHMWPE Joint Replacements. Dissertation, UC  
603 Berkeley. 2015.
- 604 [49] Invibio. PEEK-OPTIMA Natural: Typical Material Properties [Internet]. 2013 [cited 2016  
605 Apr 18]. Available from: [https://invibio.com/library?id=%7B9ec81b92-8ab8-40da-af8f-  
606 6c3bf002aa84%7D](https://invibio.com/library?id=%7B9ec81b92-8ab8-40da-af8f-6c3bf002aa84%7D)
- 607 [50] Invibio. PEEK-OPTIMA Reinforced: Mechanical Properties, Physical Properties and  
608 Biocompatibility [Internet]. 2014 [cited 2016 Apr 18]. Available from:  
609 <https://invibio.com/library?id=%7B4957faed-3d7d-466b-bed0-f8dfcf1a6e5a%7D>
- 610 [51] Lafdi K, Wright M. Carbon fibers. In: Peters S, editor. Handbook of Composites. London:  
611 Chapman & Hall; 1998. p. 169–201.
- 612